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(12) **United States Patent**
Armani et al.

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(54) **CLICK CHEMISTRY SURFACE
FUNCTIONALIZATION FOR RESONANT
MICRO-CAVITY SENSORS**

(58) **Field of Classification Search**

CPC G01N 21/7746; G01N 2021/7789;
G01N 33/54353

See application file for complete search history.

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U.S.C. 154(b) by 0 days.

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Chao et al. Polymer microring resonators for biochemical sensing
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Nov. 26, 2008, now Pat. No. 8,092,855.

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28, 2007.

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G01N 33/547 (2006.01)

G01N 33/553 (2006.01)

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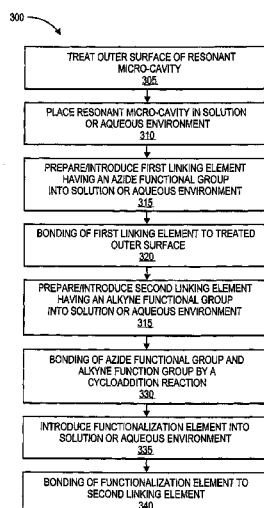
(52) **U.S. Cl.**

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(57) **ABSTRACT**

Micro-cavity resonant sensors have outer surfaces that are
functionalized using click chemistry, e.g., involving a
cycloaddition reaction of an alkyne functional group and an
azide functional group. A first polymer linking element binds
to an outer surface of the micro-cavity and has an azide
functional group, which bonds to an alkyne functional group
of a second polymer linking element as a result of a cycload-
dition reaction. A functionalization element such as an anti-
body, antigen or protein for sensing a target molecule is bound
to the second linking element.

21 Claims, 28 Drawing Sheets



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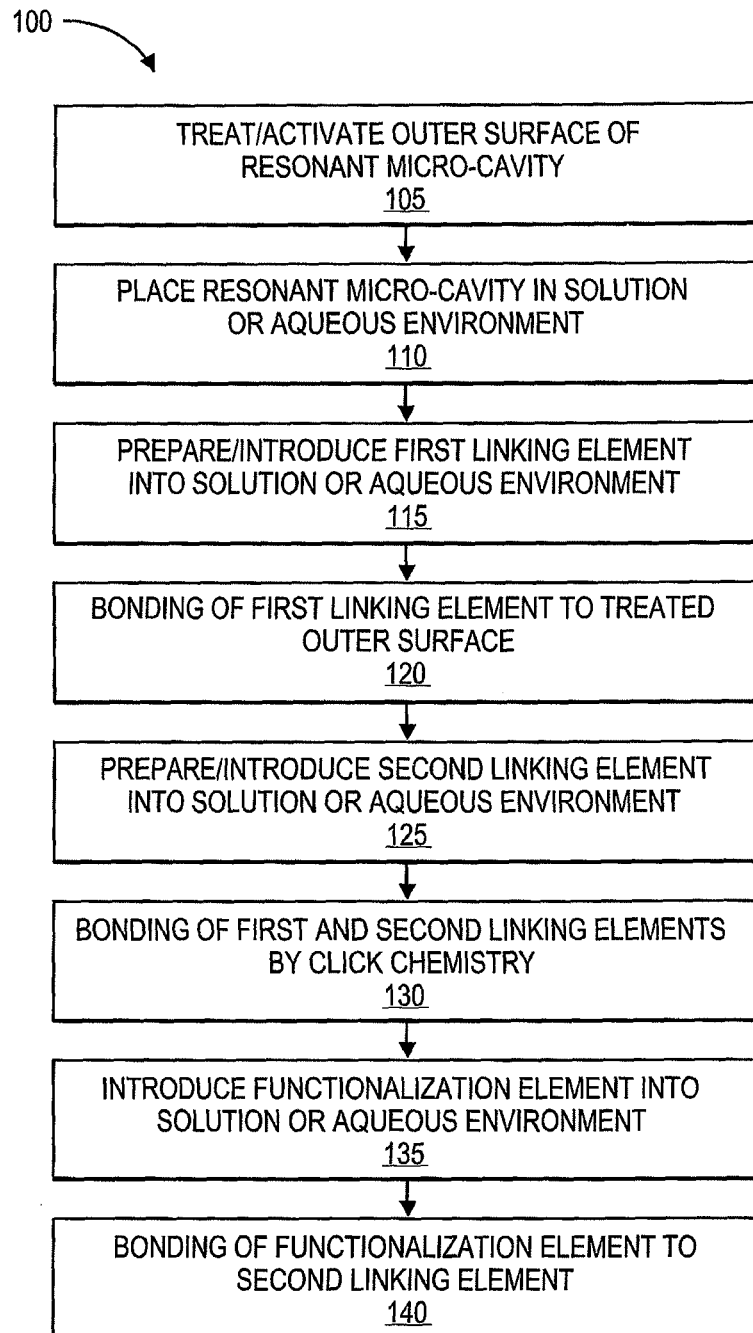
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**FIG. 1**

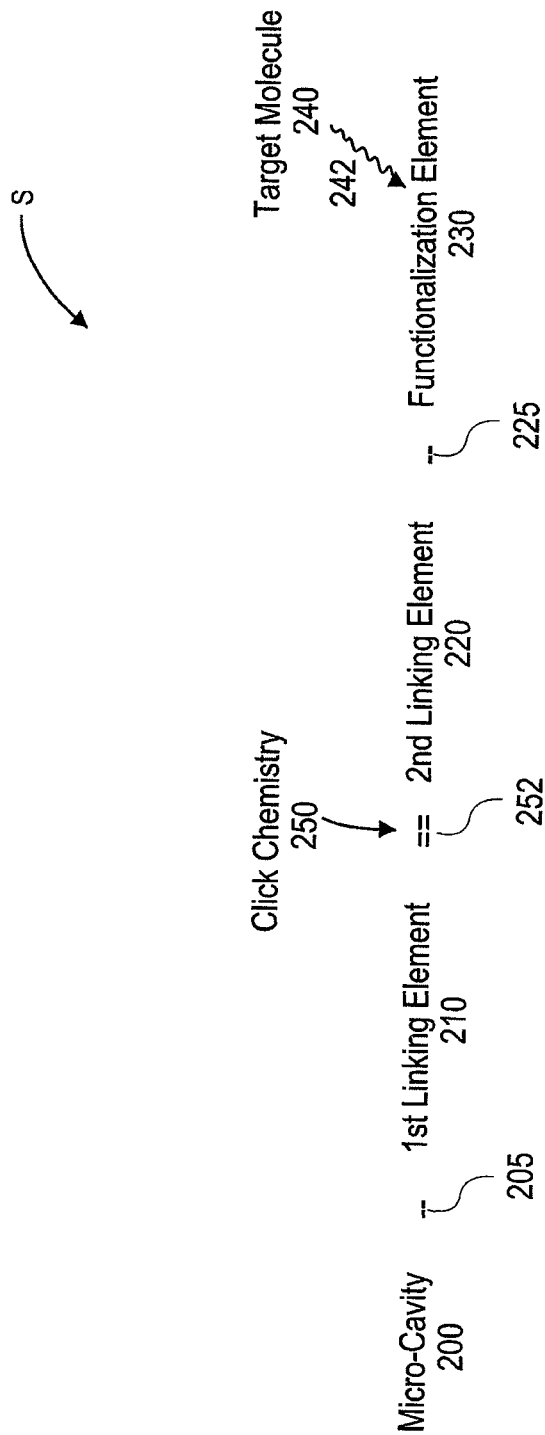


FIG. 2A

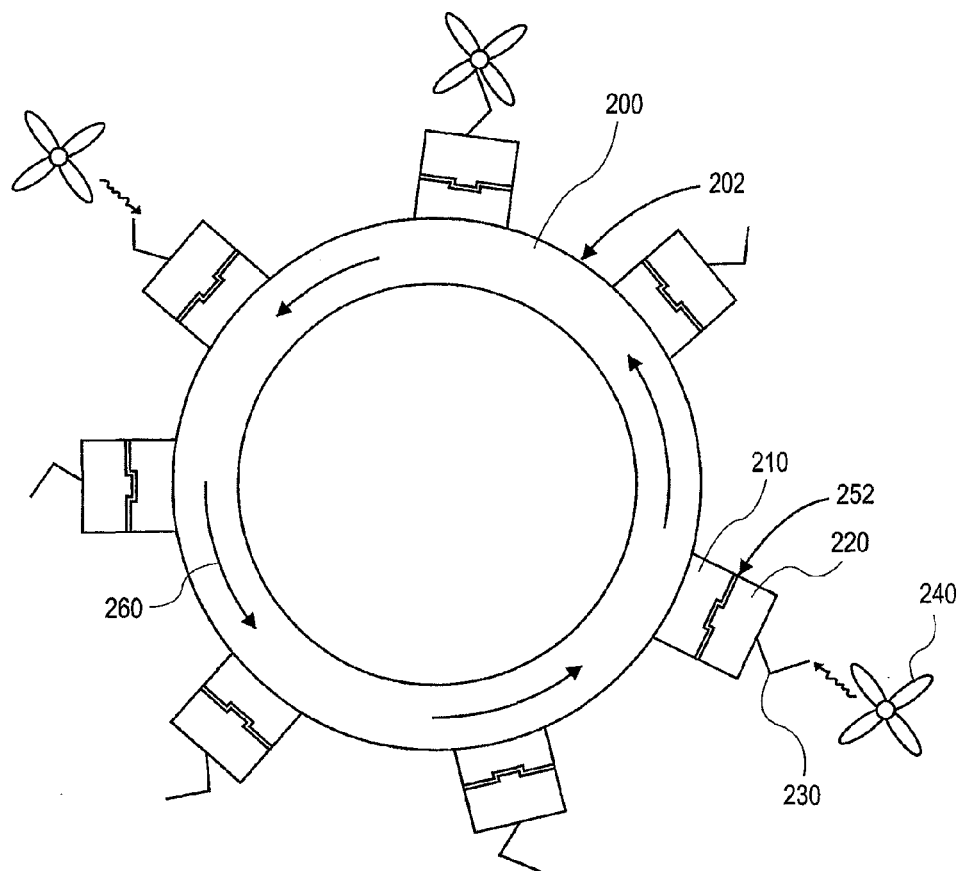


FIG. 2B

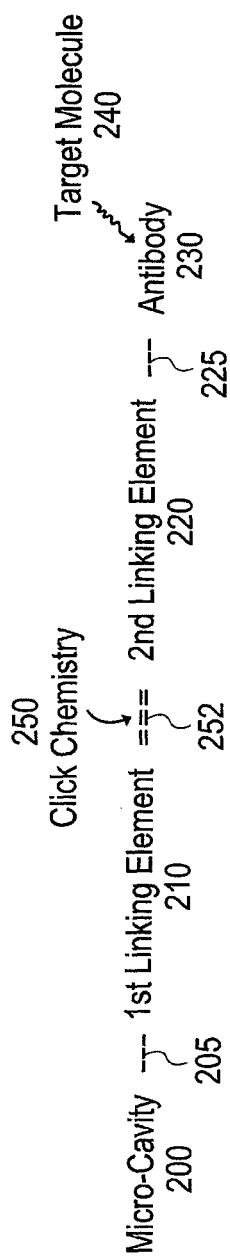


FIG. 2C

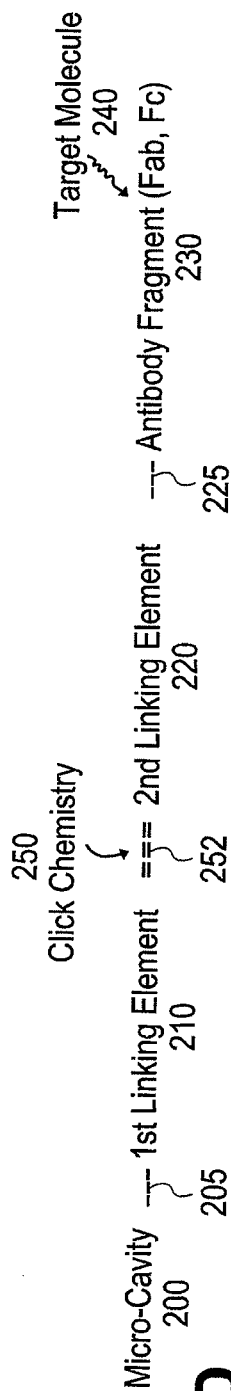


FIG. 2D

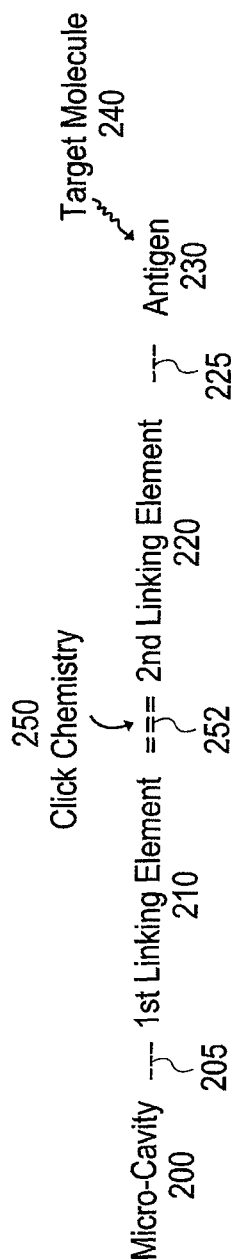


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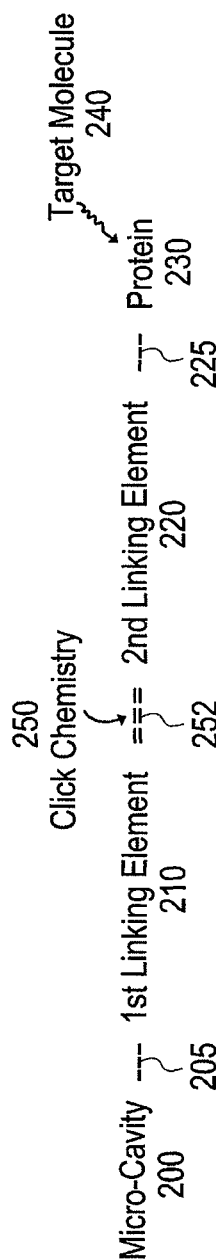
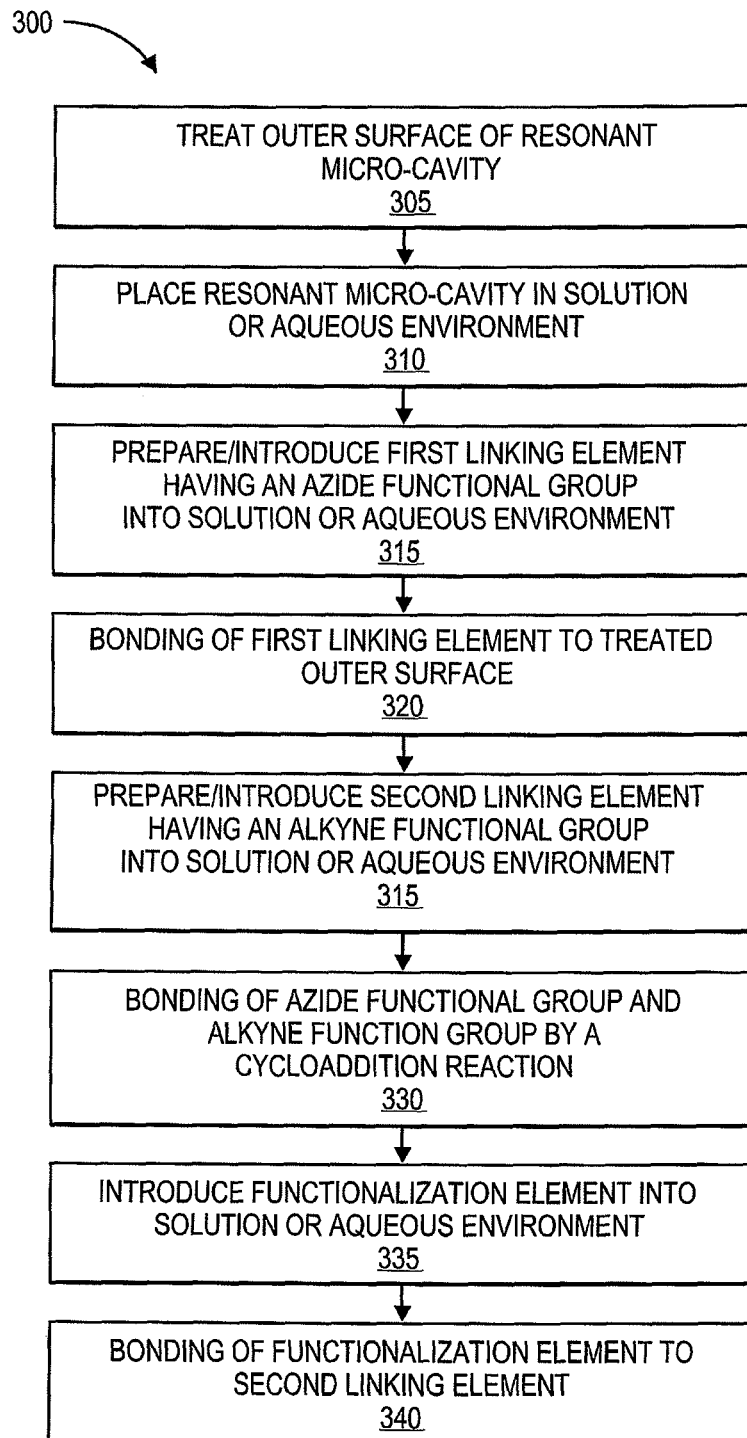


FIG. 2F

**FIG. 3**

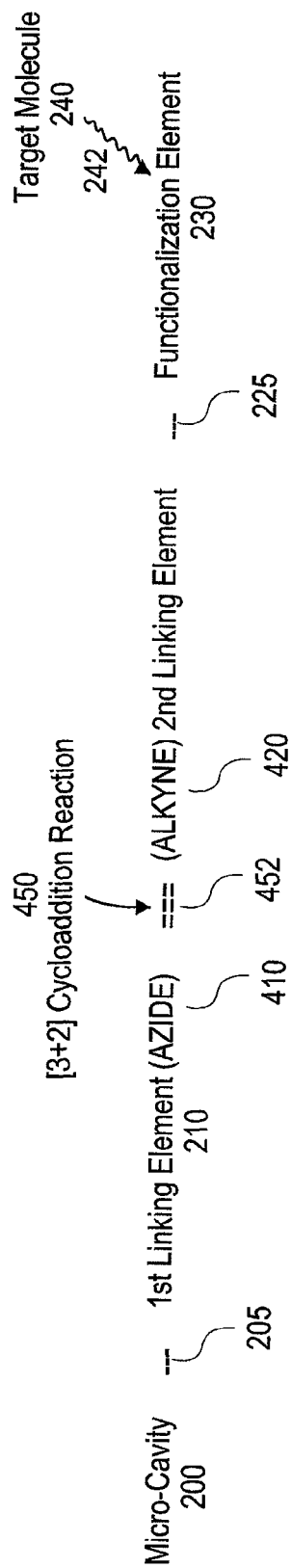


FIG. 4A

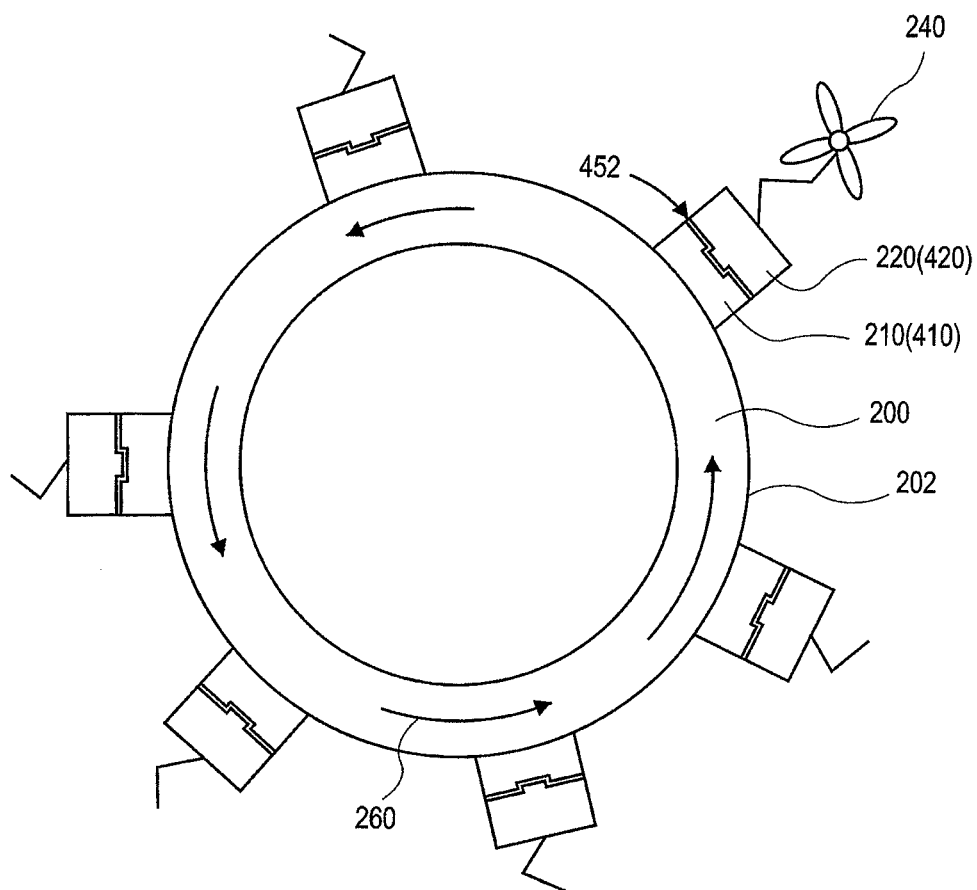
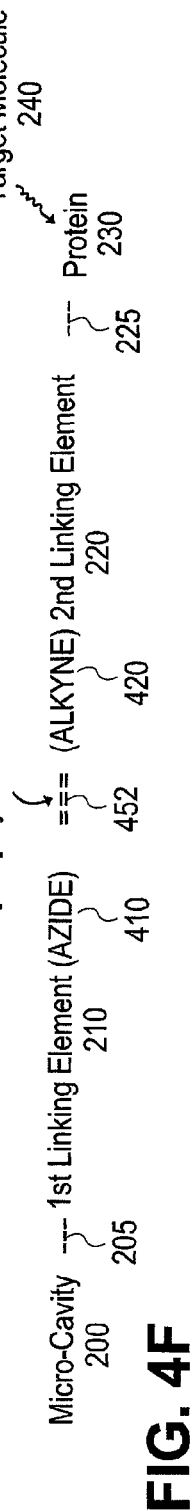
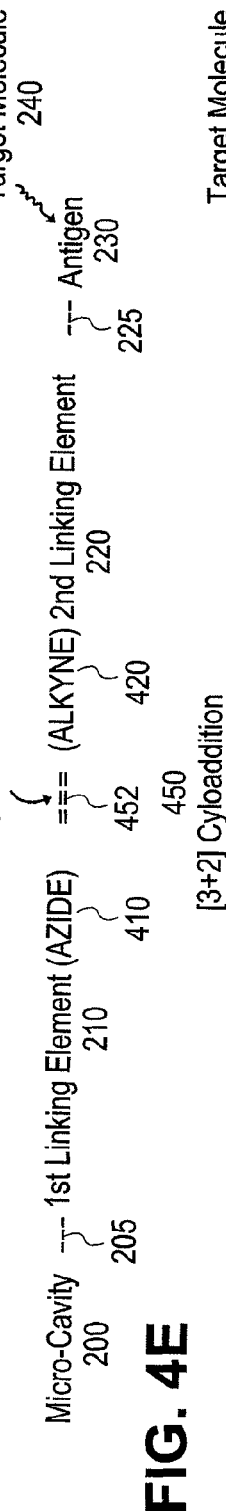
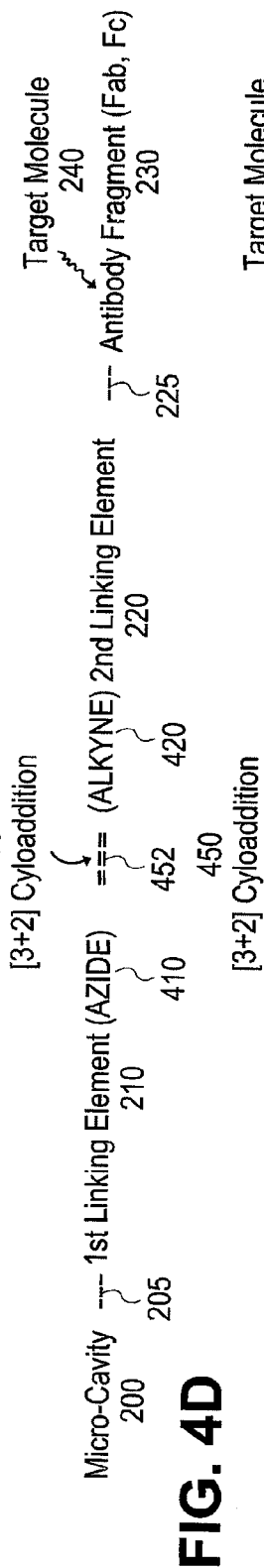
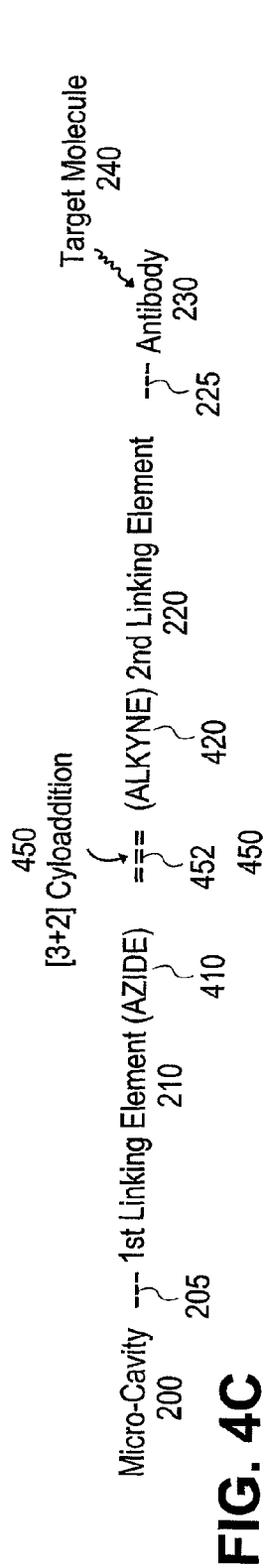
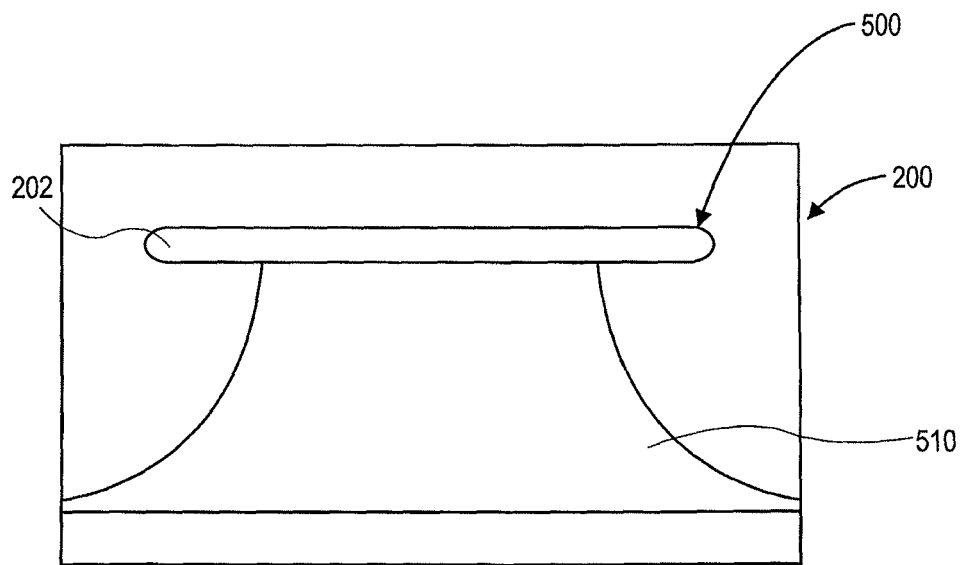
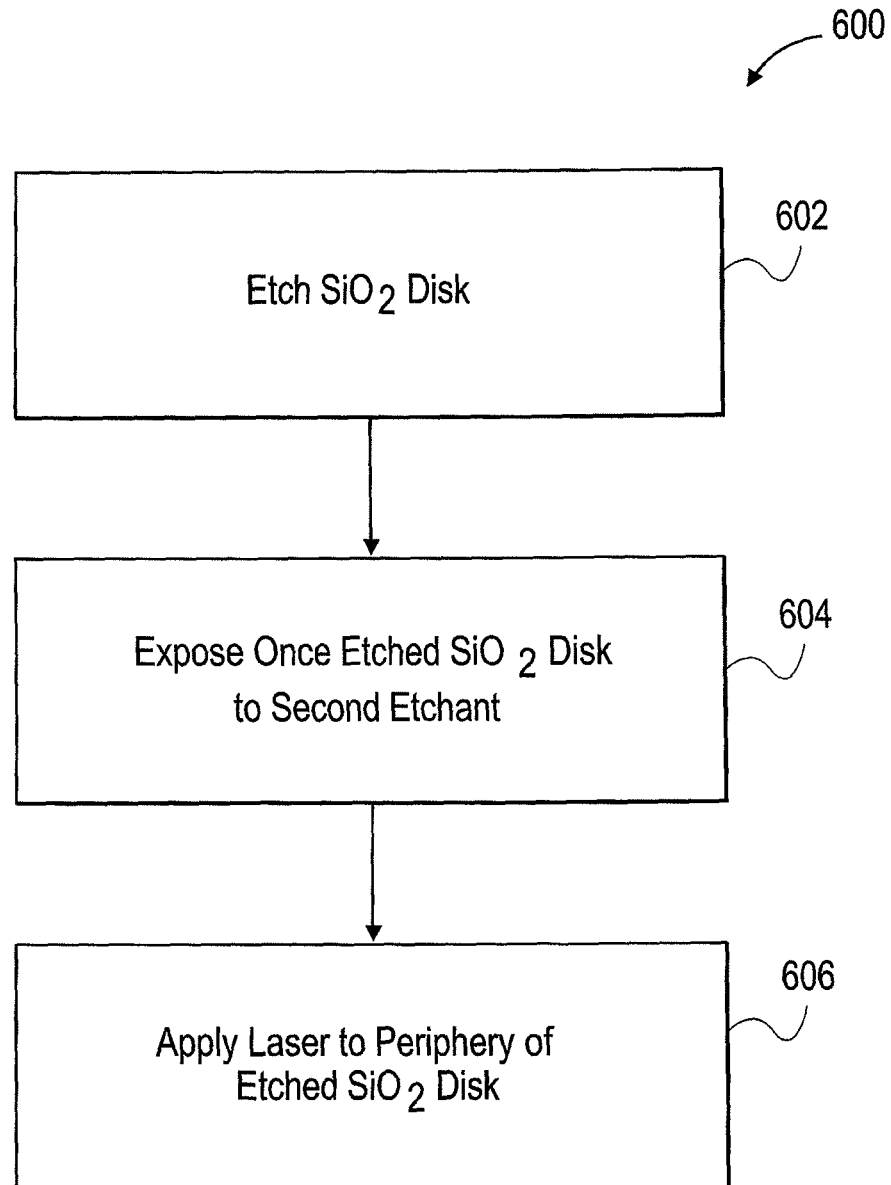
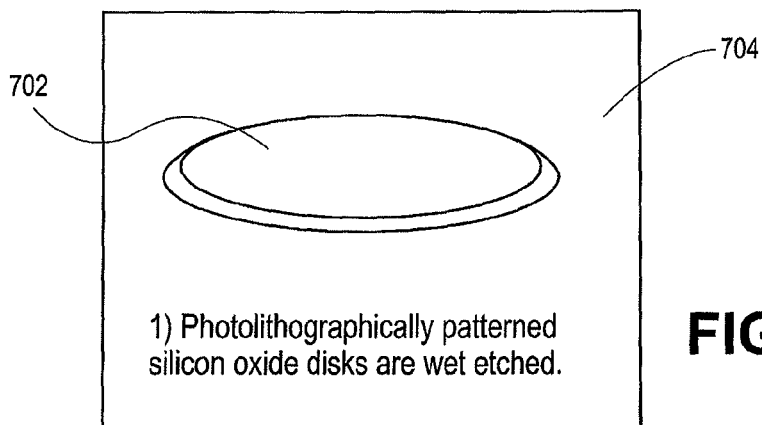
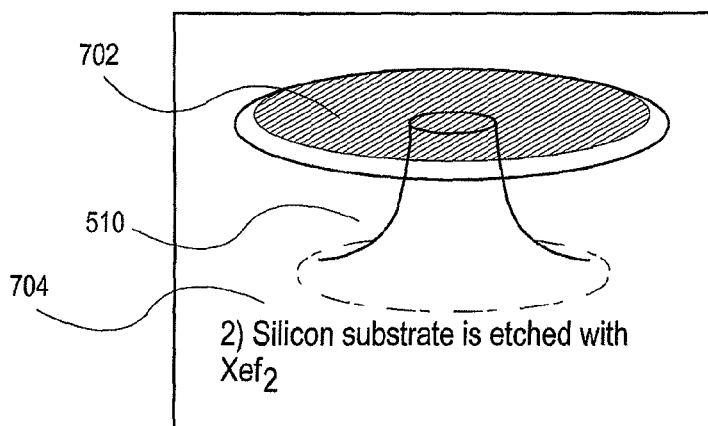
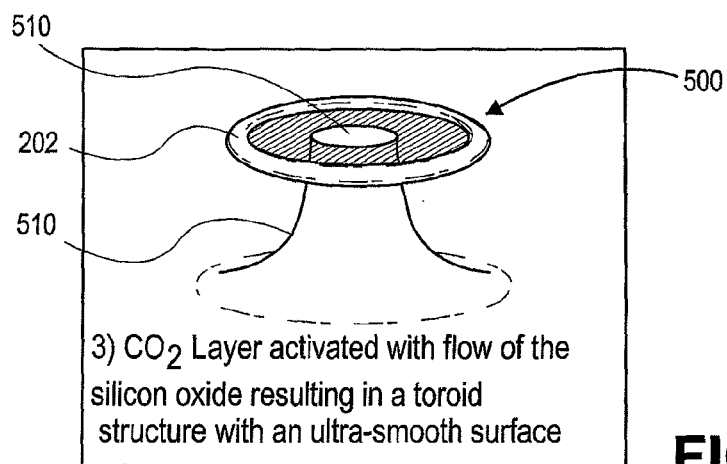


FIG. 4B



**FIG. 5**

**FIG. 6**

**FIG. 7A****FIG. 7B****FIG. 7C**

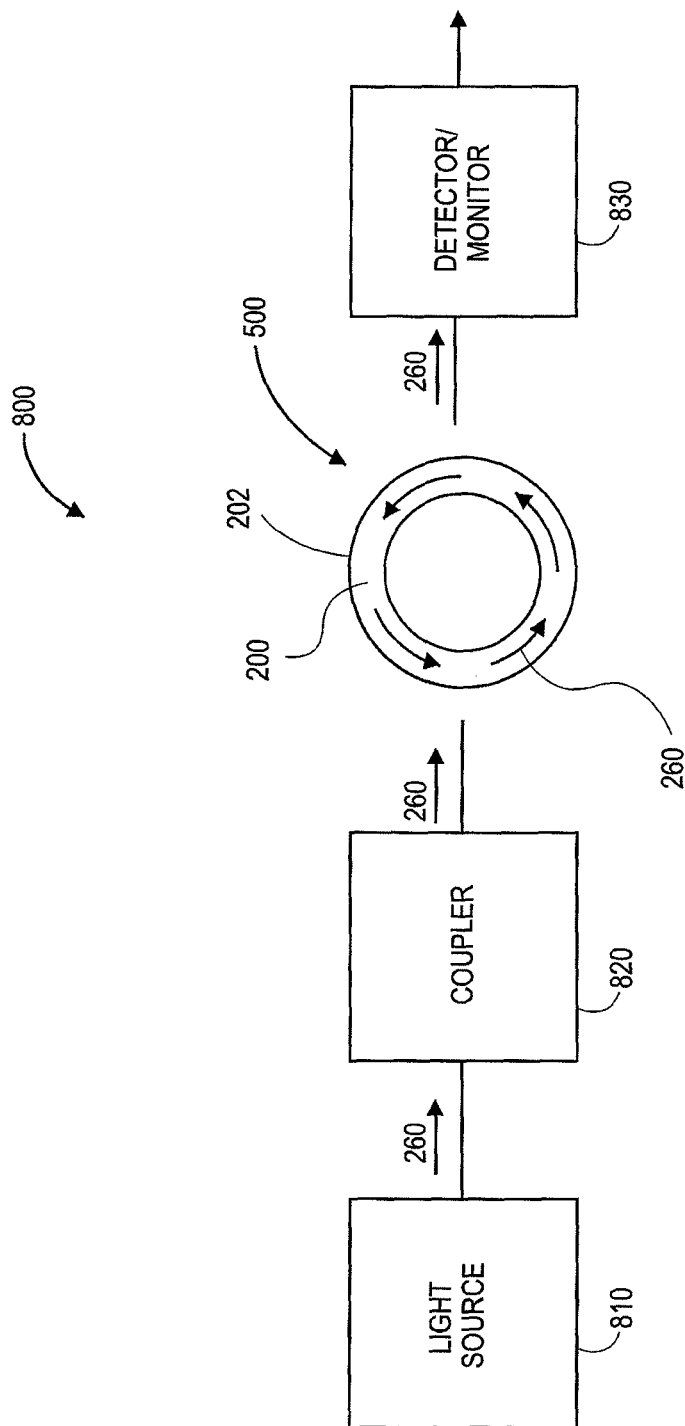


FIG. 8

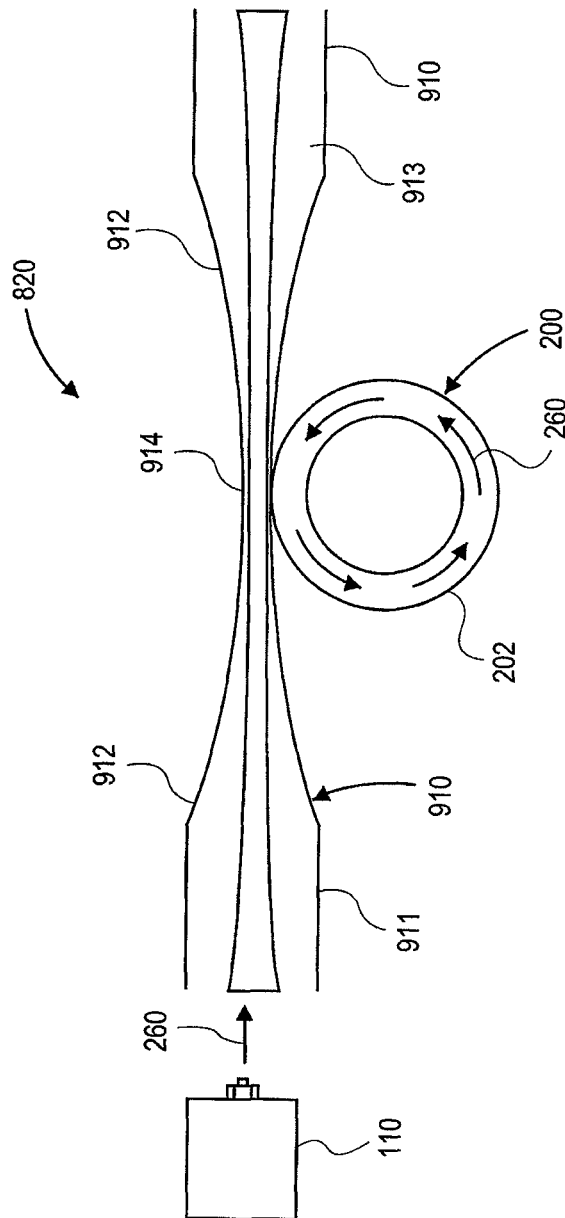


FIG. 9

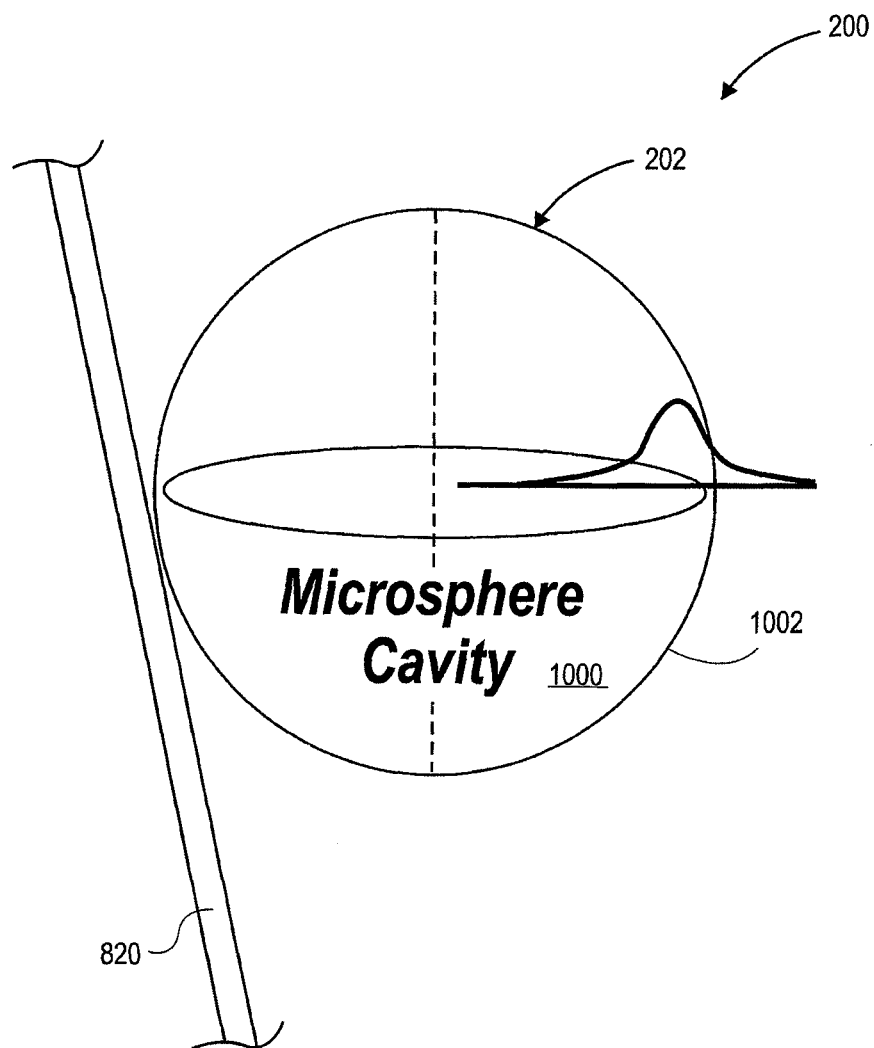
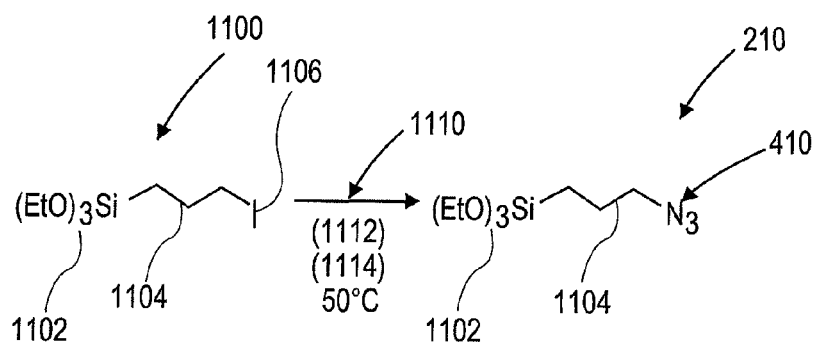
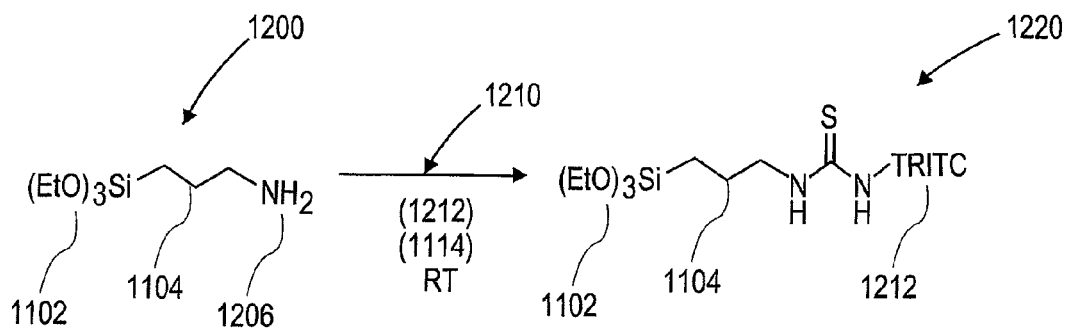
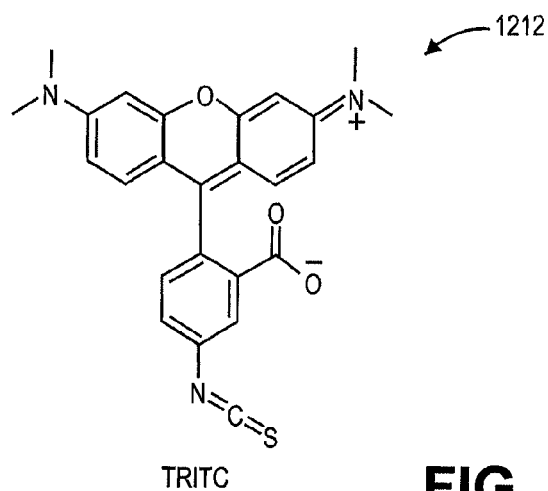
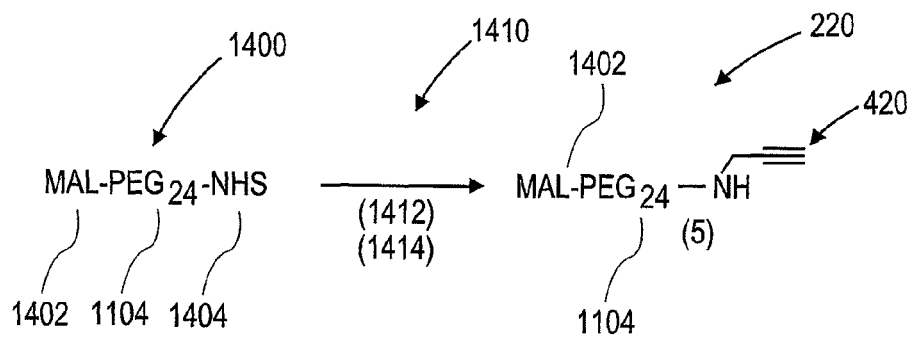
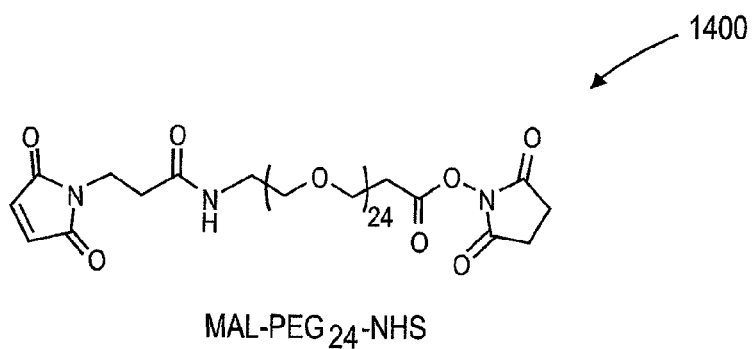


FIG. 10

**FIG. 11****FIG. 12**

**FIG. 13****FIG. 14****FIG. 15**

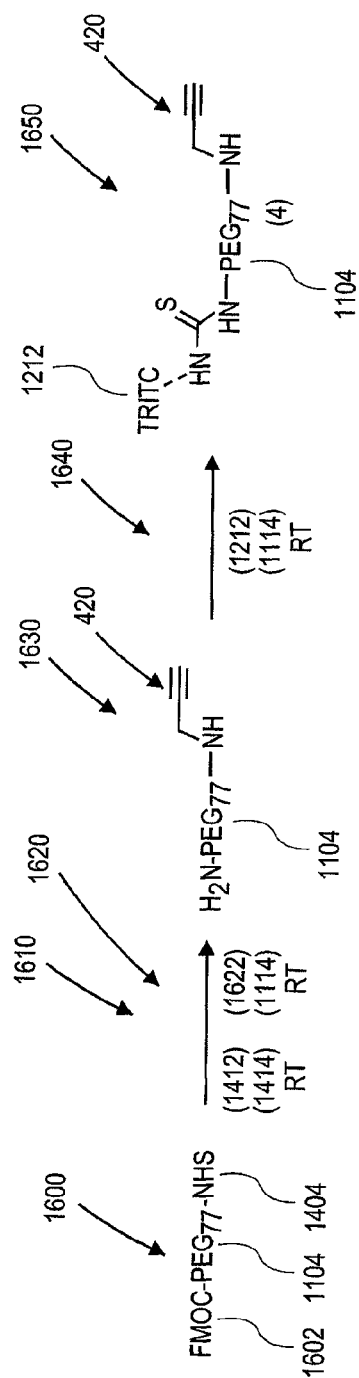


FIG. 16

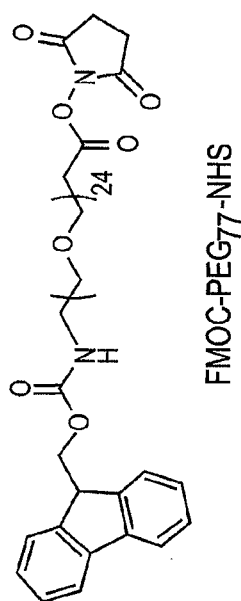


FIG. 17

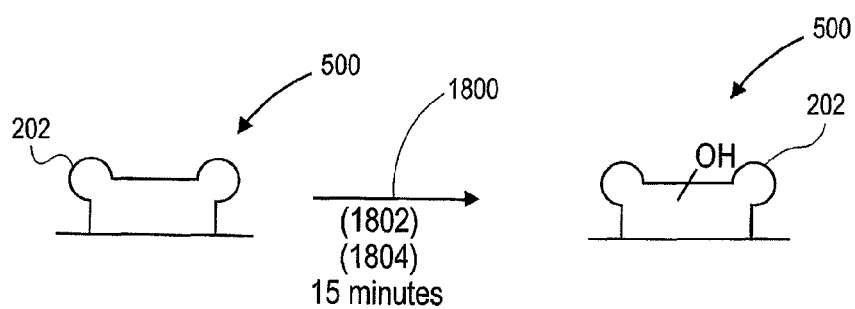


FIG. 18

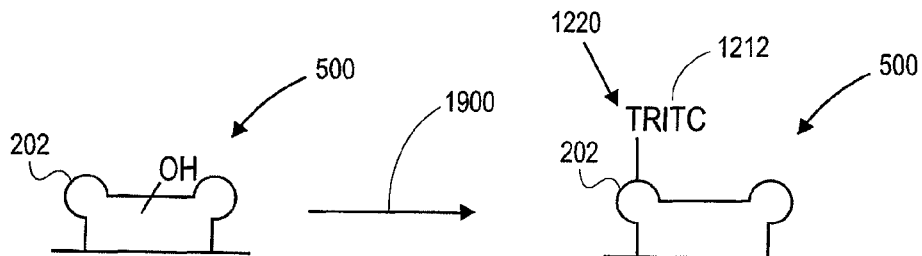


FIG. 19

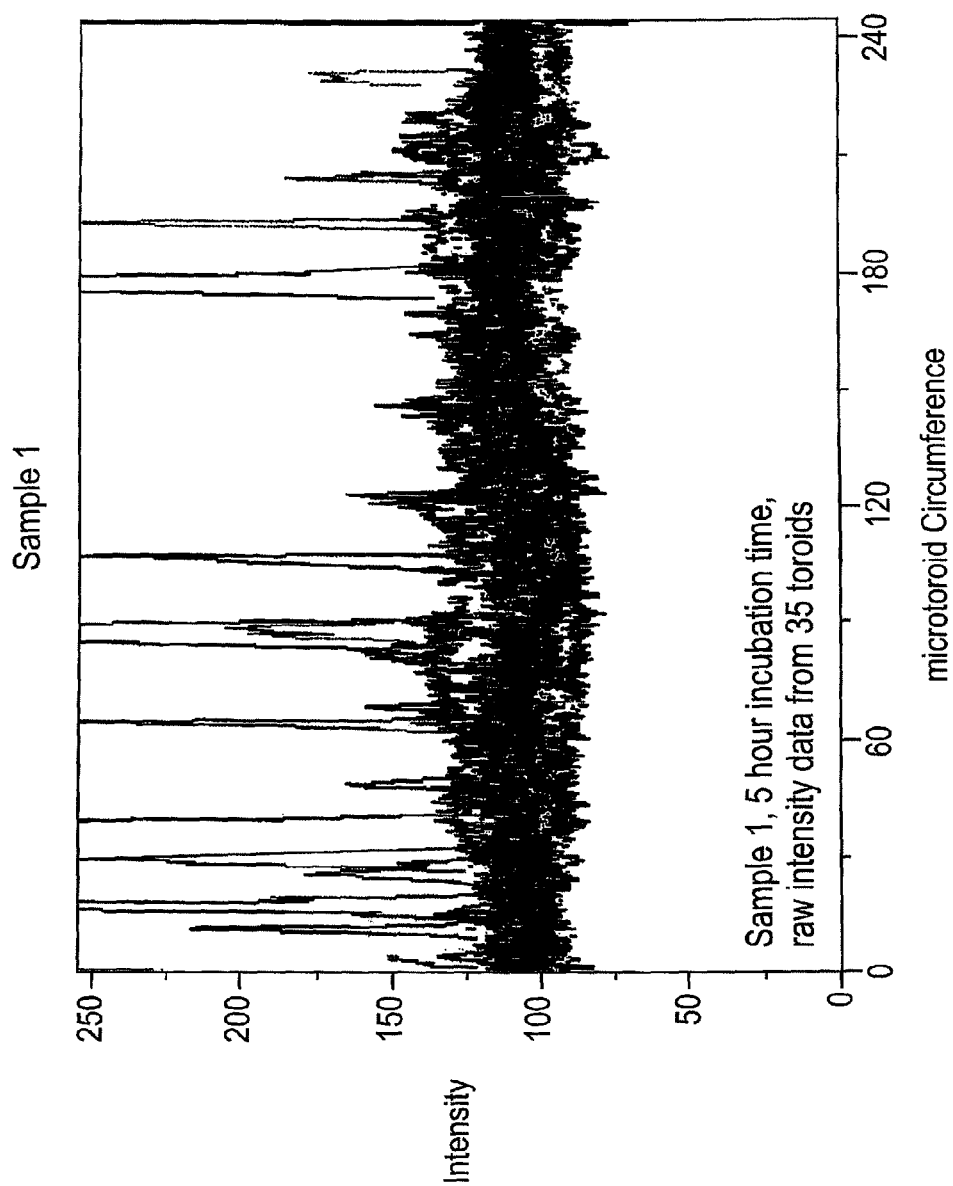


FIG. 20A

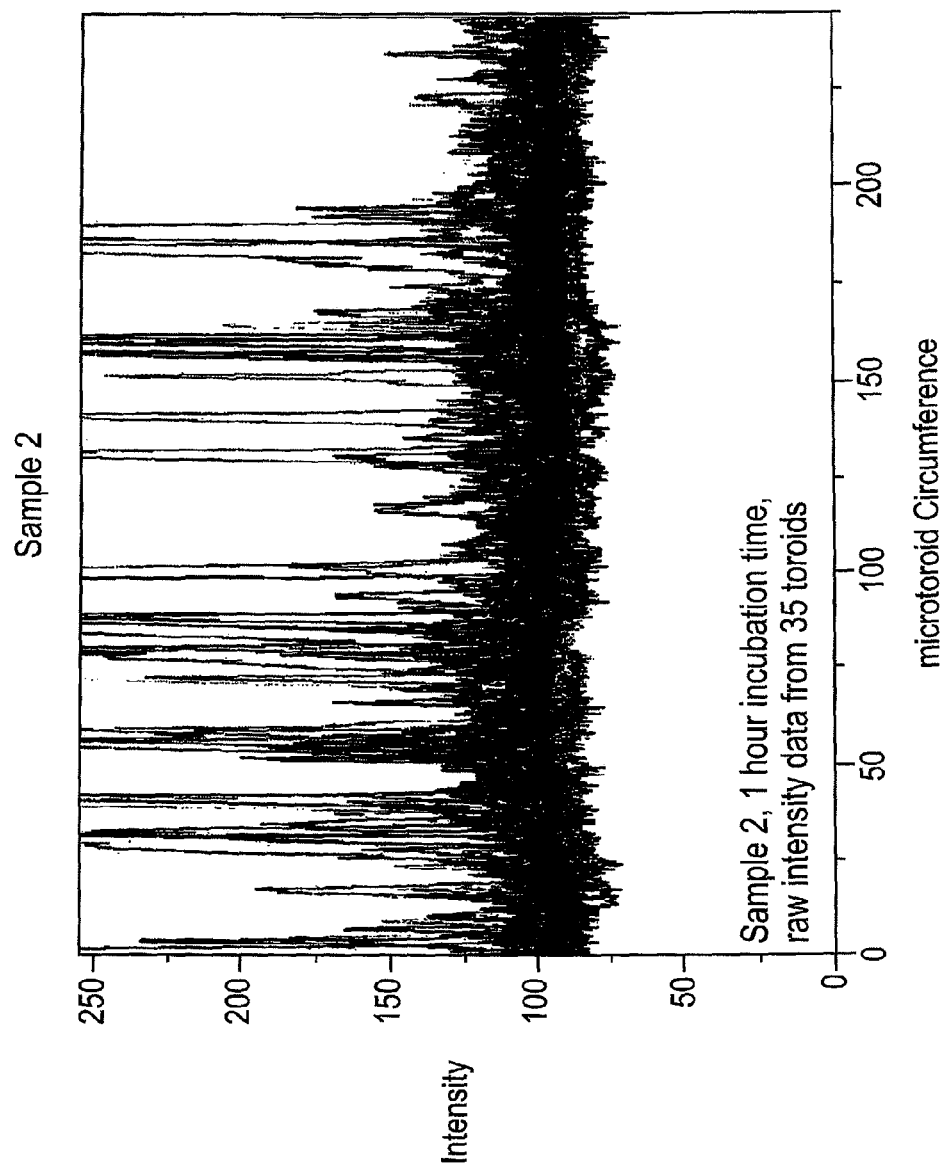


FIG. 20B

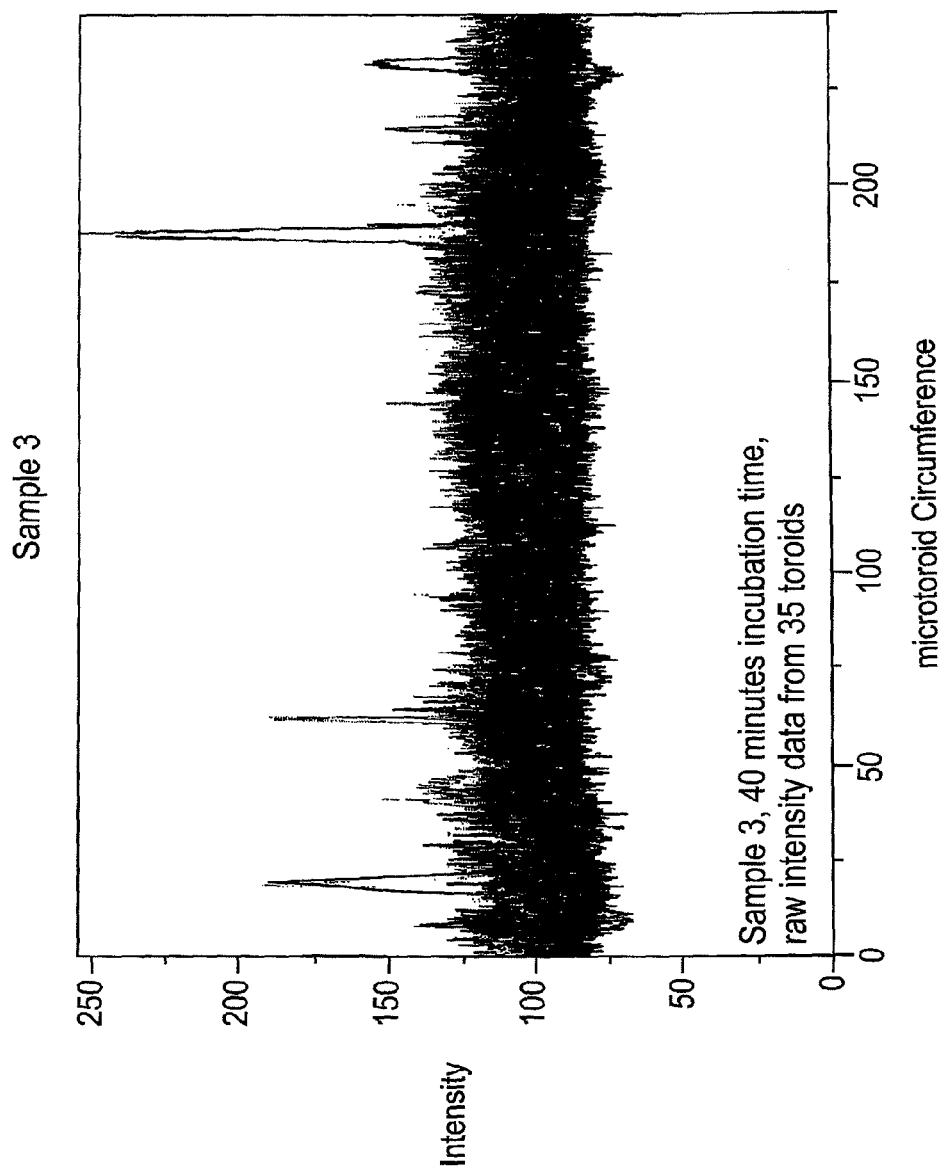
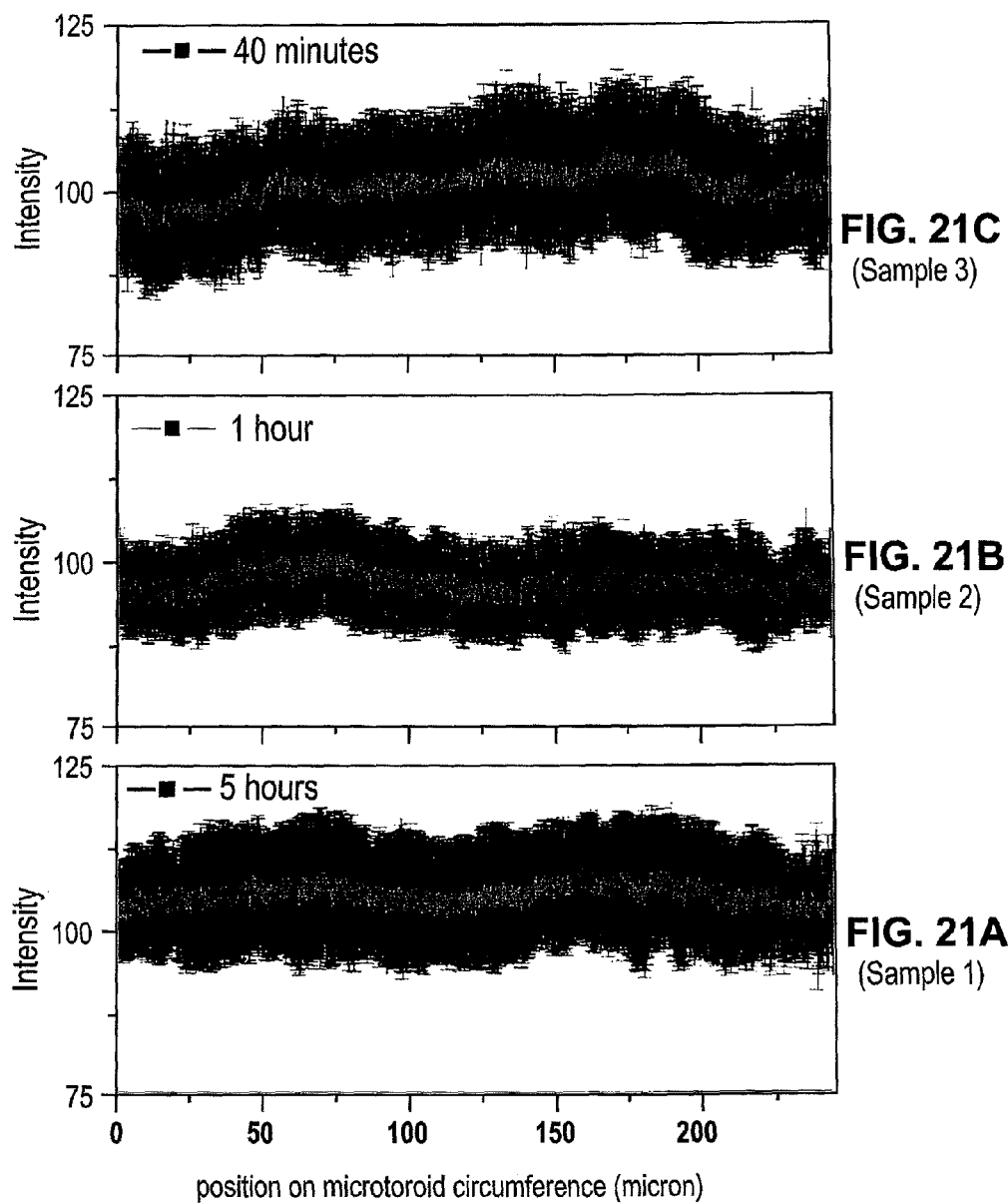


FIG. 20C



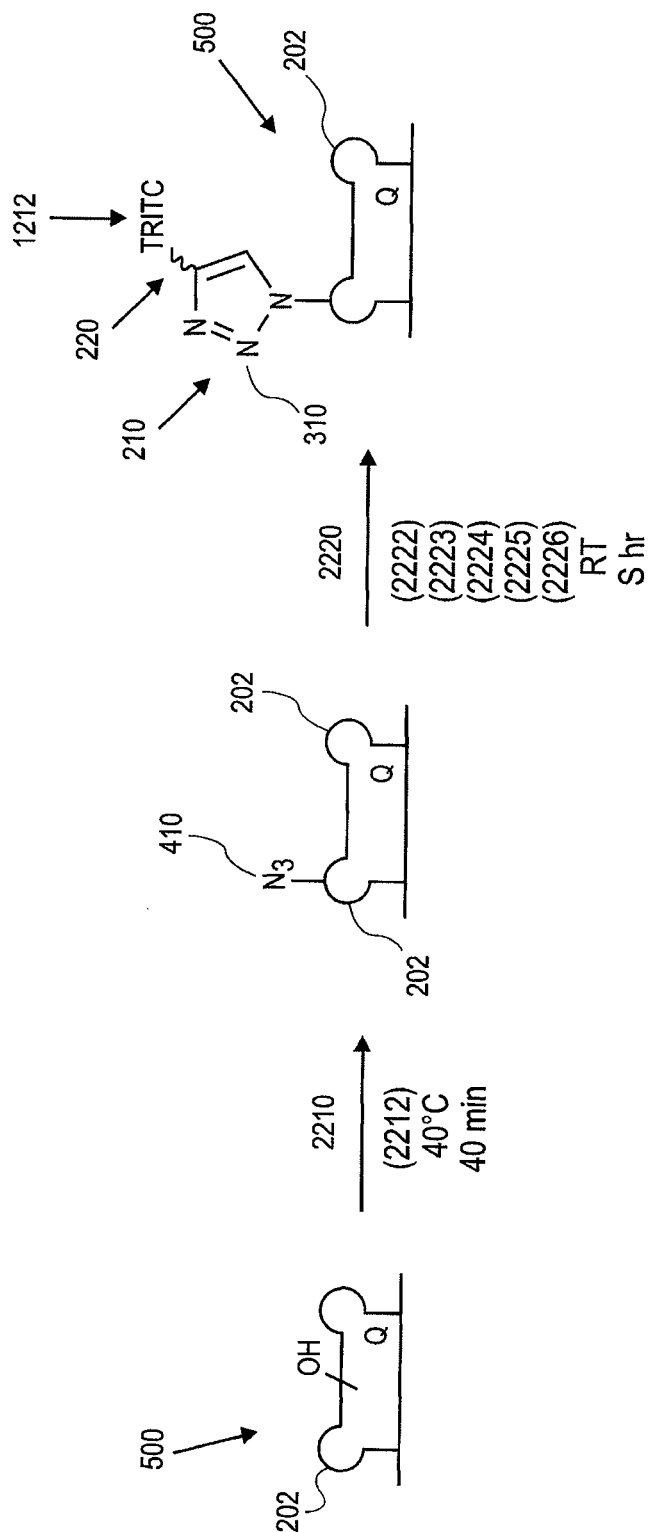


FIG. 22

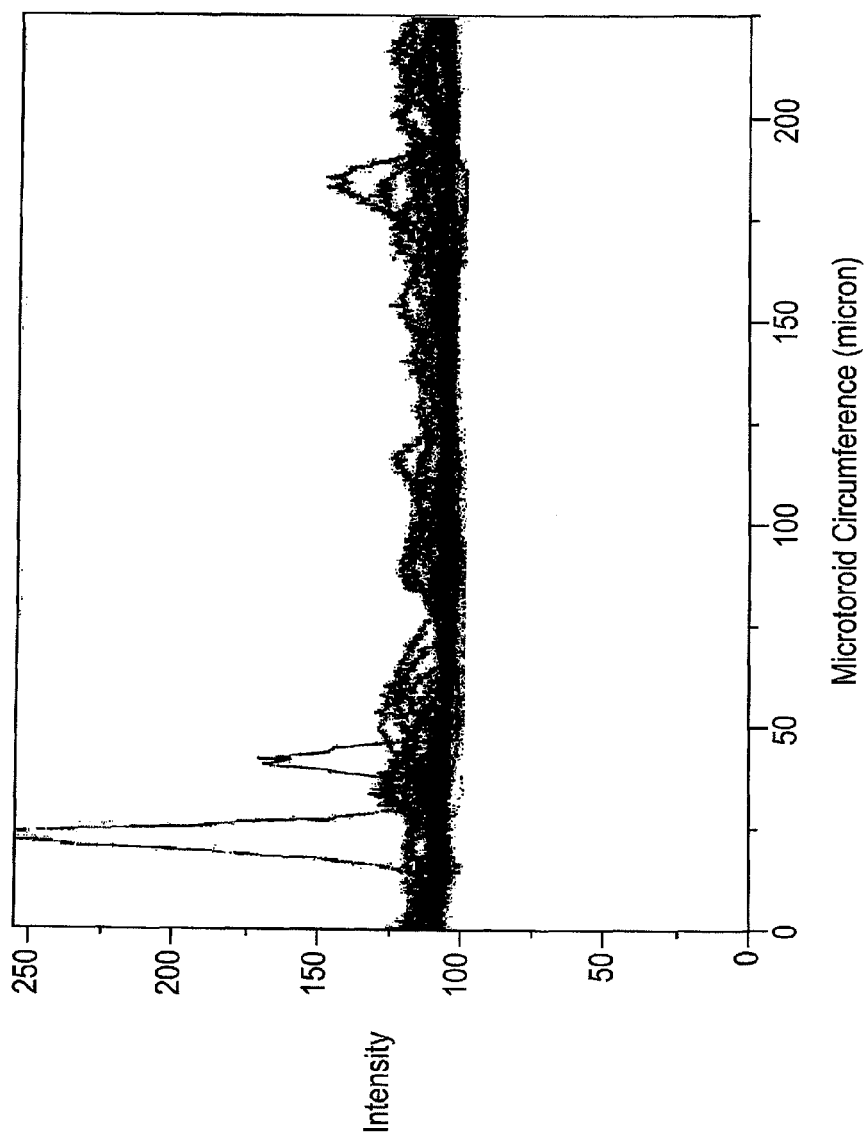


FIG. 23A

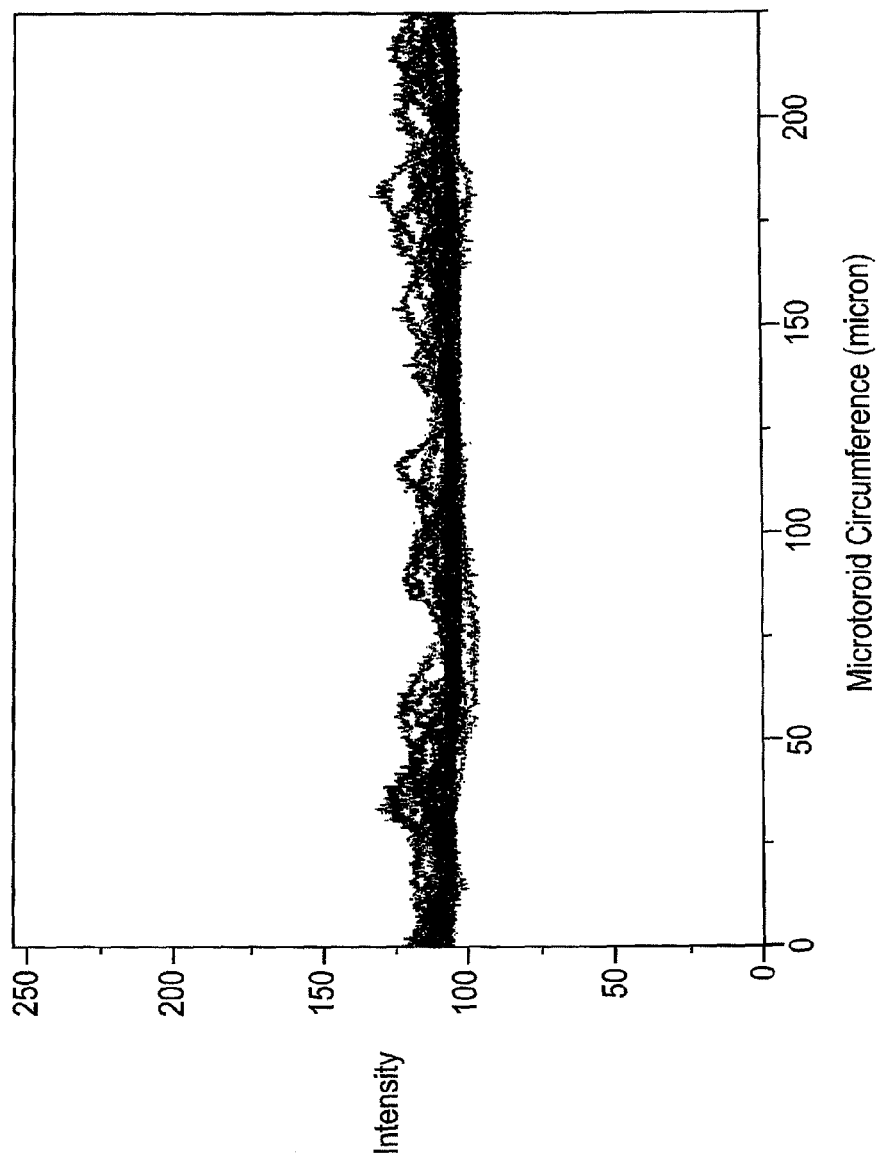
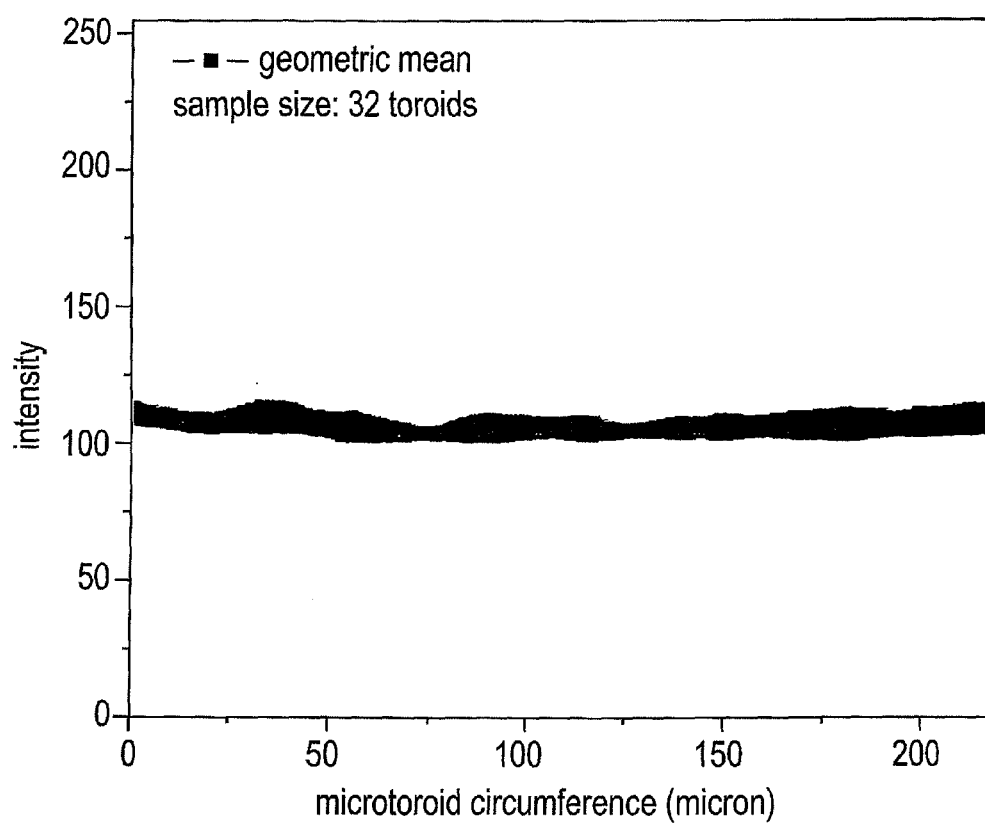


FIG. 23B

**FIG. 23C**

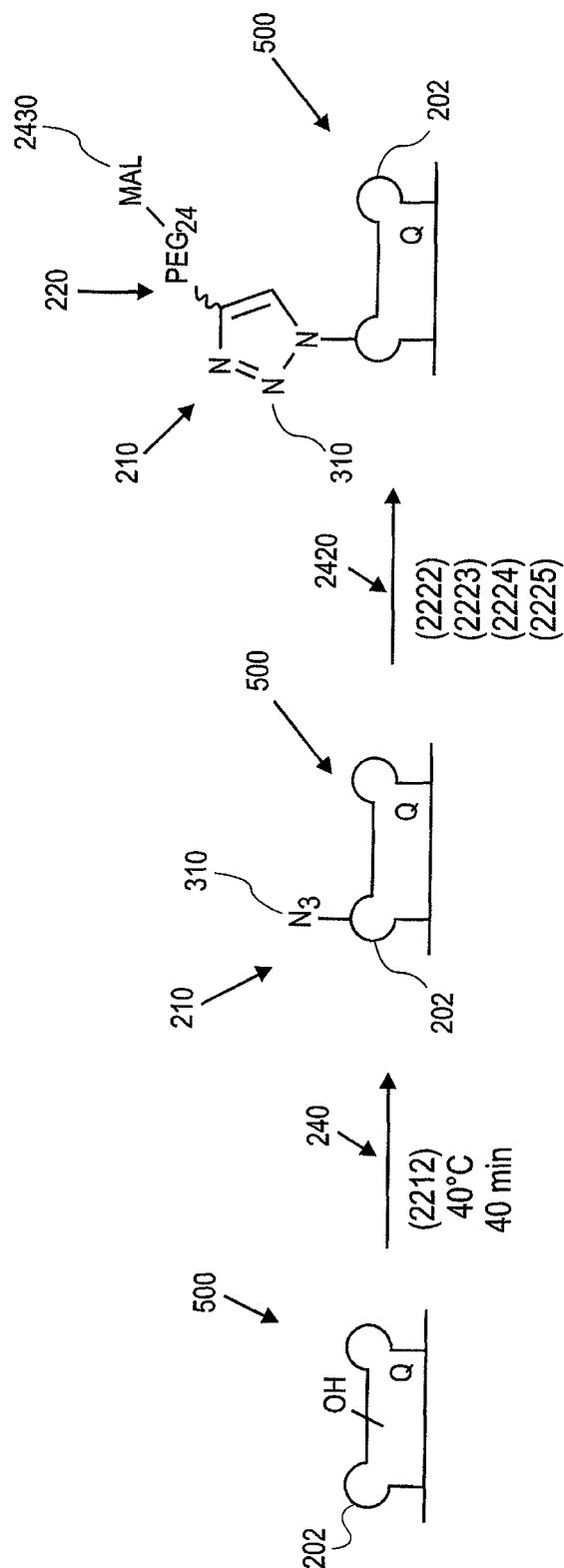
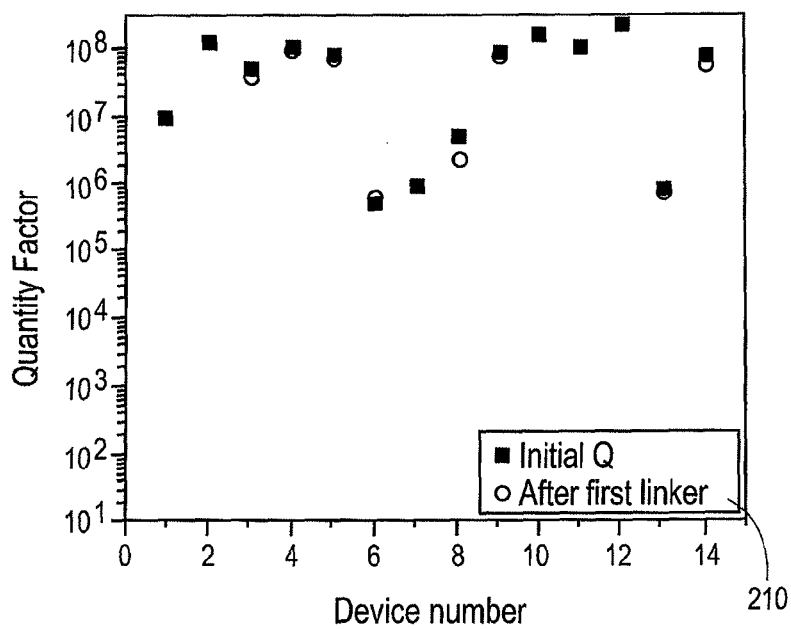
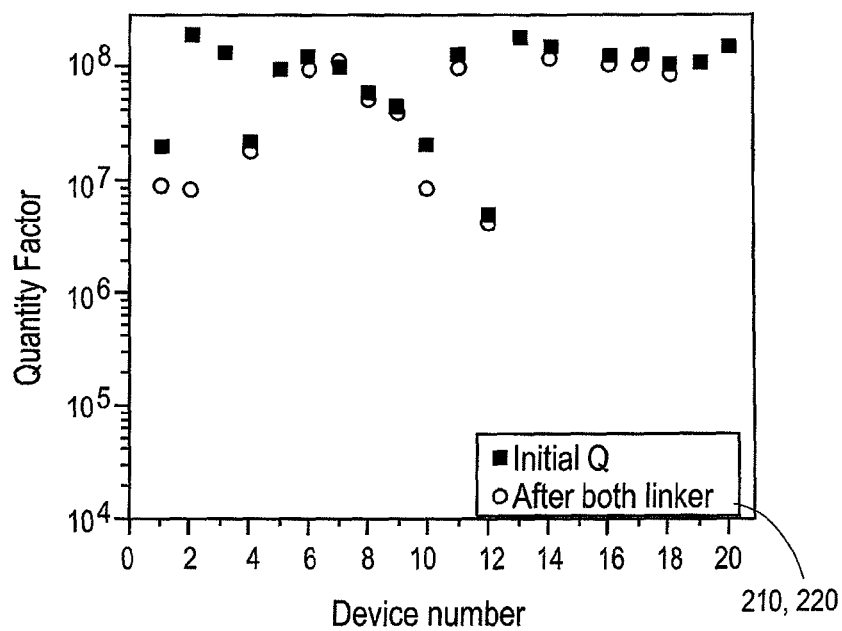


FIG. 24

**FIG. 25A****FIG. 25B**

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CLICK CHEMISTRY SURFACE FUNCTIONALIZATION FOR RESONANT MICRO-CAVITY SENSORS

RELATED APPLICATION DATA

The present application is a continuation of U.S. patent application Ser. No. 12/324,605, filed on Nov. 26, 2008, which claims the benefit under 35 U.S.C. §119 of U.S. Provisional Patent Application Ser. No. 61/004,580, filed on Nov. 28, 2007, the contents of which are incorporated herein by reference as though set forth in full.

This application may also be related to the following applications and patent, the contents of which are also incorporated herein by reference as though set forth in full: U.S. application Ser. No. 12/243,580, filed on Oct. 1, 2008; U.S. application Ser. No. 11/733,480, filed on Apr. 10, 2007; U.S. application Ser. No. 11/016,067, filed on Dec. 17, 2004; and U.S. application Ser. No. 10/678,354, filed on Oct. 2, 2003, and U.S. Pat. No. 6,583,399, issued on Jun. 24, 2003.

STATEMENT REGARDING FEDERALLY SPONSORED RESEARCH

The U.S. Government has certain rights in this invention pursuant to Grant No. HR 0011-04-1-0032 awarded by DARPA.

FIELD OF INVENTION

The present invention relates to micro-cavity sensors and sensing methods.

BACKGROUND

Various sensor devices and methods have been utilized to detect target molecules or particulates. Certain sensors involve detection or measurement of biological elements utilizing antibody-antigen interactions. While such sensors may have high specificity, they may have a number of limitations including inadequate sensitivity and the need to utilize labels.

More particularly, certain known sensors require attachment of a label to molecules that are to be detected. This requires prior knowledge of the presence of the target molecule. As a result, known label-based sensor systems are not suitable for blind or label-free detection. Further, use of labels may require additional data processing and ensemble averaging of large numbers of cells. Such processing may confuse or dull recorded responses.

Certain sensors are highly sensitive and capable of detecting a small number of molecules. For example, two known single molecule detection methods include surface enhanced raman spectroscopy (SERS) and total internal reflection fluorescence microscopy (TIRF). However, labels are needed to detect single molecules using these methods. More particularly, a gold surface is used in SERS to amplify a signal corresponding to a single labeled molecule, and with TIRF, a fluorescent label is excited and detected using a single photon camera. Such methods, however, may not be suitable for detecting single molecules in the absence of these labels.

Several sensor devices have been proposed for label-free detection including fiber optic waveguides, nanowires, nanoparticle probes, biochips, mechanical cantilevers and microsphere resonators. Examples of such known devices are described in U.S. Pat. No. 4,071,753 to Fulenwider et al., U.S. Pat. No. 4,419,895 to Fuller and U.S. Pat. No. 6,583,399 to Painter et al. While certain known devices may provide label-

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free detection capabilities, they have a number of limitations and may not be suitable for various applications and may present integration challenges.

Certain known sensors having functionalized outer surfaces for purposes of selective sensing or detection applications. Such sensors, however, may utilize surface functionalization elements and methods that involve weak bonds that are unable to retain target molecules to the functionalized surface, thereby reducing the effectiveness of the sensor. Other known sensors may have stronger bonds but are silane-based, do not form uniform monolayers, lack high binding efficiency, have limited stability in air or an ambient environment, must be stored in a buffer solution and/or have limited shelf lives and storage restrictions.

SUMMARY

One embodiment is directed to a method for preparing a resonant micro-cavity for use as a sensor, e.g., a label-free sensor. The method comprises functionalizing an outer surface of the surface of the resonant micro-cavity utilizing click chemistry.

Another embodiment is directed to a method for functionalizing a resonant micro-cavity for use as a sensor, e.g., a label-free sensor. The method comprises introducing a first linking element that bonds to an outer surface of the resonant micro-cavity and has a first functional group, and introducing a second linking element having a second functional group. A bond forms between the first functional group and second functional groups as a result of a cycloaddition reaction. The method further comprises introducing a functionalization element for selectively binding a target molecule for sensing or detecting the target molecule, the functionalization element bonding to the second linking element. Embodiments may involve a sequence in which the first linking element binds to the outer surface, the second linking element binds to the first linking element, and the functionalization element binds to the second linking element, or other sequences. For example, in other embodiments, a first linking element binds to the outer surface, and the second linking element, which already has a functionalization element bound thereto, binds to the first linking element. In yet another embodiment, the first linking element, to which a second linking element having an attached functionalization element binds, binds to the outer surface of the micro-cavity.

A further embodiment is directed to a method for functionalizing a resonant micro-cavity for use as a sensor, e.g., a label-free sensor. The method comprises introducing a first polymer linking element that binds to an outer surface of the resonant micro-cavity and has an azide functional group. The first polymer linking element has a molecular weight greater than 100. The method further comprises introducing a second polymer linking element having an alkyne functional group that bonds to the azide functional group of the first polymer linking element as a result of a cycloaddition reaction. The second polymer linking element also has a molecular weight greater than 100. The method further comprises introducing a functionalization element for selectively binding a target molecule to enable sensing or detection of the target molecule, the functionalization element bonding to the second linking element.

According to another embodiment, a resonant micro-cavity sensor comprises a resonant micro-cavity, first and second linking elements, and a functionalization element for sensing a target molecule. The resonant micro-cavity has an outer surface to which the first linking element is bound. The sec-

ond linking element is bound to the first linking element by click chemistry, and the functionalization element is bound to the second linking element.

According to yet another embodiment, a resonant micro-cavity sensor comprises a resonant micro-cavity, first and second linking elements having respective first and second functional groups, and a functionalization element for selectively binding a target molecule to enable sensing or detection of the target molecule. The resonant micro-cavity has an outer surface to which the first linking element is bound. A bond is formed between the first functional group and the second functional group as a result of a cycloaddition reaction, and the functionalization element is bound to the second linking element.

In accordance with a further alternative embodiment, a resonant micro-cavity sensor comprises a resonant micro-cavity, first and second polymer linking elements, and a functionalization element, which provides for selectively binding a molecule for detecting or sensing the molecule. The resonant micro-cavity has an outer surface to which a first polymer linking element having a molecular weight greater than 100 and an azide functional group is bound. The second polymer linking element has a molecular weight greater than 100 and an alkyne functional group. The azide and alkyne functional groups bond to each other as a result of a cycloaddition reaction. The functionalization element is bound to the second polymer linking element.

A further embodiment is directed to a method for detecting or sensing a target molecule. The method comprises introducing optical energy into a resonant micro-cavity having an outer surface that is functionalized utilizing click chemistry. The method further comprises sensing or detecting the target molecule based on or as a result of a change of an optical property of optical energy resonating within the micro-cavity.

Another embodiment is directed to method for detecting or sensing a target molecule. The method comprises introducing optical energy into a resonant micro-cavity having an outer surface that is functionalized by introducing a first linking element that bonds to the outer surface of the resonant micro-cavity and has a first functional group, introducing a second linking element having a second functional group, a bond forming between the first functional group and second functional groups as a result of a cycloaddition reaction. The method further comprises introducing a functionalization element for selectively binding a target molecule for detecting or sensing the target molecule, the functionalization element bonding to the second linking element. The method further comprises detecting the target molecule based on or as a result of a change of an optical property of optical energy resonating within the micro-cavity.

A further alternative embodiment is directed to a method for detecting a target molecule and comprises introducing optical energy into a resonant micro-cavity having an outer surface that is functionalized by introducing a first polymer linking element that bonds to an outer surface of the resonant micro-cavity and has an azide functional group, the first polymer linking element having a molecular weight greater than 100. The method further comprises introducing a second polymer linking element having an alkyne functional group that bonds to the azide functional group of the first polymer linking element as a result of a cycloaddition reaction, the second polymer linking element having a molecular weight greater than 100, and introducing a functionalization element for sensing a target molecule, the functionalization element bonding to the second linking element. The method further comprises sensing or detecting the target molecule based on

or as a result of a change of an optical property of optical energy resonating within the micro-cavity.

In one or more embodiments, a first linking element bonds to the outer surface of the resonant micro-cavity and the second linking element bonded thereto form a single substantially uniform layer. A first linking element and a second linking element are covalently bonded to each other by click chemistry, e.g., by cycloaddition of an azide group of the first linking element and an alkyne group of the second linking element.

In at least one embodiment, a functionalization element for selecting binding a target molecule to enable detection or sensing of the target molecule is bound to a second linking element and may be an antibody, an antibody fragment, an antigen or a protein for use in detecting various target molecules.

In one or more embodiments, one or more linking elements are made of a polymer, such as polyethylene glycol (PEG), polyethylene oxide (PEO) or another suitable polymer, e.g., a polymer having a molecular weight greater than 100. For example, the molecular weight of a polymer chain of the first linking element may be greater than about 300, and a molecular weight of a polymer chain of the second linking element may be greater than 1500.

In at least one embodiment, the micro-cavity of a sensor or that is involved in a functionalization or sensing method may be various shapes, be made of different materials and have various Q values. In certain embodiments, the micro-cavity is made of silica and is planar, e.g., a silica toroid-shaped micro-cavity. In certain embodiments, a substrate may support the micro-cavity, such as a toroid-shaped or other planar micro-cavity, and an outer edge of the resonant micro-cavity extends outwardly beyond a top of the substrate. In other embodiments, the micro-cavity is a spheroid or micro-sphere.

In one or more embodiments, the micro-cavity has a Q factor much greater than 10^6 , e.g., greater than 10^8 . With embodiments, high or ultra-high Q factors provide high sensitivity and provide for the ability to detect a small number of molecules and even an individual molecule while the functionalized outer surface provides for high specificity.

BRIEF DESCRIPTION OF THE DRAWINGS

The foregoing and other aspects of embodiments will be understood with reference to the detailed description of illustrated embodiments in conjunction with the accompanying drawings, wherein:

FIG. 1 is a flow chart of a method for functionalizing an outer surface of a resonant micro-cavity using click chemistry according to one embodiment;

FIG. 2A further illustrates bonding of different components using surface functionalization based on click chemistry;

FIG. 2B generally illustrates a top view of a toroid-shaped resonant micro-cavity having an outer surface that is functionalized using click chemistry;

FIGS. 2C-F illustrate bonding of different components, linking elements and functionalization elements that may be utilized in embodiments illustrated in FIGS. 2A-B, wherein FIG. 2C illustrates use of an antibody functionalization element, FIG. 2D illustrates use of an antibody fragment functionalization element, FIG. 2E illustrates use of an antigen functionalization element, and FIG. 2F illustrates use of a protein functionalization element;

FIG. 3 is a flow chart of a method for functionalizing an outer surface of a resonant micro-cavity using a cycloaddition reaction according to one embodiment;

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FIG. 4A further illustrates bonding of different components using surface functionalization based on a cycloaddition reaction of an azide functional group and an alkyne functional group according to one embodiment;

FIG. 4B generally illustrates a top view of a toroid-shaped resonant micro-cavity having an outer surface that is functionalized utilizing a cycloaddition reaction;

FIGS. 4C-F illustrates bonding of different components, linking elements and functionalization elements that may be utilized in embodiments illustrated in FIGS. 4A-B, wherein FIG. 4C illustrates use of an antibody functionalization element, FIG. 4D illustrates use of an antibody fragment functionalization element, FIG. 4E illustrates use of an antigen functionalization element, and FIG. 4F illustrates use of a protein functionalization element;

FIG. 5 is a side view of a toroid-shaped resonant micro-cavity having an outer surface that may be functionalized utilizing click chemistry or a cycloaddition reaction according to embodiments illustrated in FIGS. 1-4F;

FIG. 6 is a flow diagram illustrating a method of manufacturing a toroid-shaped micro-cavity as shown in FIG. 5;

FIGS. 7A-C further illustrate fabrication stages of the method shown in FIG. 6;

FIG. 8 illustrates a sensor system constructed according to one embodiment that includes a resonant micro-cavity having an outer surface that is functionalized according to embodiments illustrated in FIGS. 1-4F;

FIG. 9 illustrates an example of a coupler or waveguide in the form of a fiber taper coupler that may be utilized with embodiments;

FIG. 10 illustrates a spherical micro-cavity or micro-sphere having an outer surface that may be functionalized using click chemistry or a cycloaddition reaction according to embodiments illustrated in FIGS. 1-4F;

FIG. 11 illustrates synthesis of a first linking element having an azide functional group for use in embodiments;

FIG. 12 illustrates synthesis of a fluorescently labeled counterpart to the first linking element shown in FIG. 11 and that is utilized to verify the effectiveness of embodiments;

FIG. 13 illustrates a structure of a TRITC molecule of the fluorescently labeled counterpart illustrated in FIG. 12;

FIG. 14 illustrates synthesis of a second linking element having an alkyne functional group for use in embodiments;

FIG. 15 illustrates the molecular structure of a starting material of the embodiment illustrated in FIG. 14;

FIG. 16 illustrates synthesis of a fluorescently labeled counterpart to the second linking element shown in FIG. 14 and that is utilized to verify the effectiveness of embodiments;

FIG. 17 illustrates the molecular structure of the starting material of the fluorescently labeled counterpart illustrated in FIG. 16;

FIG. 18 illustrates treatment of an outer surface of a resonant micro-cavity in preparation for bonding of a fluorescently labeled counterpart to a first linking element to the outer surface;

FIG. 19 illustrates bonding of a fluorescently labeled counterpart to a first linking element to an outer surface treated as shown in FIG. 18 for purposes of analyzing the uniformity of bonding of the first linking element to different circumferential positions on the outer surface of the micro-cavity using fluorescence intensity testing;

FIGS. 20A-C are graphs illustrating fluorescence intensity test results and data of bonding of fluorescently labeled counterparts to a first linking element as shown in FIG. 19 and that were synthesized using three different methods;

FIGS. 21A-C are graphs further illustrating fluorescence intensity test results of bonding of fluorescently labeled coun-

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terparts to a first linking element as shown in FIG. 19 and that were synthesized using three different methods;

FIG. 22 illustrates a fluorescently labeled counterpart to embodiments having first and second linking elements for purposes of analyzing the uniformity of bonding of the first and second linking elements to different circumferential positions on the outer surface of the micro-cavity using fluorescence intensity testing;

FIGS. 23A-C are graphs illustrating fluorescence intensity test results and data of bonding of the fluorescently labeled counterpart shown in FIG. 22 to different circumferential positions on the outer surface of the micro-cavity;

FIG. 24 illustrates bonding of first and second linking elements to an outer surface of a micro-cavity and bonding of malamite for use in binding to functionalization elements;

FIGS. 25A-B are graphs illustrating Q factor tests utilizing the resonant micro-cavities functionalized as shown in FIG. 24, wherein FIG. 25A illustrates Q factor data for a number of different micro-cavities before and after attachment of the first linking element having the azide functional group, and FIG. 25B illustrates Q factor data for a number of different micro-cavities before and after attachment of both of the first and second linking elements.

DETAILED DESCRIPTION OF ILLUSTRATED EMBODIMENTS

Embodiments of the invention are related to methods for functionalizing a surface of a resonant micro-cavity for use as a sensor and resulting resonant micro-cavity sensors having a functionalized surface and label-free or blind detection or sensing methods, including label-free or blind detection or sensing of single or individual molecules. Surface functionalization embodiments are based on or utilize click chemistry, e.g., the [3+2]cycloaddition reaction (also referred to as a [1+3] cycloaddition reaction) of an azide functional group and an alkyne functional group. For example, an azide functional group of a first linking element that binds or bonds to an outer surface of a resonant micro-cavity and an alkyne of a second linking element to which a functionalization element for detecting a target molecule is attached are bonded together by click chemistry or a cycloaddition reaction.

"Click chemistry" as utilized in this specification is defined as a chemical reaction involving molecular building blocks that selectively and covalently bond or "click" together. A "cycloaddition" reaction as utilized in this specification is defined as a type of click chemistry reaction. One embodiment of the invention utilizes a 1+3-dipolar cycloaddition reaction of azide and alkyne functional groups, otherwise referred to as a [3+2]cycloaddition reaction. Other embodiments may involve other reactions including, for example, the Diels-Alder [4+2] cycloaddition reaction between a diene and a dienophile. For ease of explanation, reference is made to click chemistry or a [3+2]cycloaddition reaction.

Resonant micro-cavity sensors that are functionalized according to embodiments have high sensitivity as a result of high or ultra-high Q values and high selectivity as a result of surface functionalization by click chemistry or cycloaddition reactions. Sensor embodiments also provide for uniform, high-density covalent surface immobilization of molecules and high binding efficiencies. Such sensors also have improved environmental stability (e.g., temperature and pH) as a result of covalent bonds that provide for temperature and pH changes to controllably release target molecules and for repeat sensor use. Micro-cavity surfaces functionalized according to embodiments are also less susceptible to chemical degradation such as oxidative processes and are stable in

air. This allows sensor embodiments to be stored for longer durations and for storage flexibility. Further, given the manner in which micro-cavity surfaces are functionalized with a non-naturally occurring azide functional group, embodiments do not involve incorrect binding of naturally occurring or biological elements to unbound azide functional groups, which may otherwise occur in known devices that involve incorrect binding of biological elements and associated impaired sensor performance.

Multiple sensors having surfaces functionalized according to embodiments may form an array of sensors, and sensors in an array may have diameters, materials, shapes, Q values and functionalization elements to provide different or customized detection capabilities and detection of different target molecules. Sensors and arrays thereof may also be configured for integration on a chip and in a sampling and concentration system. Embodiments can be utilized in continuous, real-time monitoring applications and detection of particles and molecules in a solution or in air when utilizing a suitable condenser. Further, embodiments may be used in, for example, military applications, commercial and research applications including but not limited to explosives detection, process controls, cell signaling and single molecule studies, environmental monitoring, chemical detection, toxicology, medical diagnostics and other applications.

Further aspects of embodiments and applications thereof are described in further detail with reference to FIGS. 1-4F. Micro-cavities that can be functionalized according to embodiments, methods of fabrication, and detection systems in which such micro-cavity sensors may be integrated are described with reference to FIGS. 5-10. Embodiments involving a toroid-shaped resonant micro-cavity and tests thereof are described in further detail with reference to FIGS. 11-25B.

Referring to FIG. 1 and with further reference to FIGS. 2A-F, a method 100 for preparing or functionalizing a resonant micro-cavity 200 in which optical energy 260 resonates for use as a sensor (generally referred to as resonant micro-cavity or sensor 200) involves click chemistry 250, a first linking element 210 that binds or bonds to an outer surface 202 of the micro-cavity 200, and a second linking element 220 to which a functionalization element 230 is bound. The functionalization element 230 is configured for selectively binding a target molecule to enable detection of the target molecule.

In the illustrated embodiment, the functionalization method 100 involves treating or activating the outer surface 202 of the resonant micro-cavity 200 in preparation for binding or bonding of the first linking element 210 to the outer surface 202 at step 105. According to one embodiment in which the micro-cavity 200 is a silica micro-cavity, step 105 involves treating the outer surface 202 using a Piranha etch solution or other suitable surface treatment. One known Piranha etch solution that may be utilized in embodiments is a mixture of sulfuric acid (H_2SO_4) and hydrogen peroxide (H_2O_2), e.g., a solution of 70% sulfuric acid (H_2SO_4) and 30% hydrogen peroxide (H_2O_2). When a micro-cavity 200 is placed in this etch solution, e.g., for about 15 minutes, this solution hydroxylates the outer surface 202 to add OH groups thereto and to activate and prepare the outer surface 202 for binding of the first linking element 210 thereto. The micro-cavity 200 may also be made of other materials including silicon and other suitable materials, and other surface 202 treatments or treatment parameters may be utilized or adjusted as needed. Examples of other reagents or surface treatments that may be utilized with embodiments include, for example, silane-based surface functionalizations (e.g.,

trimethylchlorosilane and trimethylsilylchlorosilane) and plasma-based treatments (e.g., oxygen plasma. This specification refers to a Piranha treatment of a silica micro-cavity surface 202 for ease of explanation.

At step 110, the resonant micro-cavity 200 is placed in a solution or aqueous environment. One example of a solution that may be utilized in embodiments is a phosphate buffered saline solution (PBS) at a pH of about 7.2 to about 7.5. Such a solution may, for example, contain 50-100 mM sodium phosphate (monobasic and dibasic) and 150 mM of NaCl. Another example of a solution that may be utilized is a Tris-HCl buffer or a Citrate-phosphate buffer within the same pH range. For ease of explanation, reference is made generally to a solution or aqueous environment, but it should be understood that various solutions may be utilized.

At step 115, the first linking element 210 is synthesized or prepared (if necessary) and introduced into the solution or aqueous environment in which the resonant micro-cavity 200 is placed. As a result, at step 120, the first linking element 210 binds or covalently bonds 205 to the active or treated outer surface 202 of the silica resonant micro-cavity 200. At step 125, the second linking element 220 is synthesized or prepared (if necessary) and introduced into the solution or aqueous environment. At step 130, a covalent bond 252 is formed between the first linking element 210 and the second linking element 220 by click chemistry 250. Covalent bonds 205, 252 provide for improved environmental (temperature, pH) stability and stability against chemical degradation by processes such as oxidative processes. Embodiments are also better suited for storage and are more flexible compared to other known devices having functionalized outer surfaces with limited storage or shelf lives as a consequence of the biological elements that are utilized to functionalize known devices.

At step 135, a functionalization element 230 for sensing a target molecule 240 that binds 242 to the functionalization element 230 is introduced into the solution or aqueous environment. At step 140, the functionalization element 230 binds or bonds 225 to the second linking element 220. Although FIG. 1 illustrates a certain sequence, it should be understood that steps may occur in different orders or simultaneously.

In certain embodiments, the functionalization element 230 as illustrated in FIG. 2A is an antibody (FIG. 2C), an antibody fragment (Fab, Fc) (FIG. 2D); an antigen (FIG. 2E), or a protein (FIG. 2F). Other functionalization elements 230 may also be utilized depending on the target molecule 240 to be detected and/or the method of surface functionalization. Examples of target molecules 240 that may be detected using embodiments include, but are not limited to, DNA, mRNA, virus and bacteria.

A functionalization element 230 or probing element (such as an antibody, antigen, DNA, etc.) can be attached or linked to the second linking element 210 in various ways. For example, the functionalization element 230 usually expresses amines, carboxylic acids and alcohols from its amino acid groups that can be used as points of attachment to the second linking element 220.

In one embodiment, the functionalization element 230 includes amine groups. Different types of bonds and the associated electrophilic agents that may be employed include: Isourea and Isothiourea bonds (Isothiocyanate, Isocyanate); Amide and Sulfonamide bonds (Acyl azide, NHS Ester, Sulfonyl chloride, Anhydride, Carbodiimides); Imine and Enamine bonds (reversible Schiff base) (Aldehydes, ketones); secondary amine bond (aldehydes and ketones after reduction with $NaCNBH_3$, epoxides and oxiranes); Carbamate linkage (Carbonates); Arylating agents (Aryl halides); and Amidine Linkage (Imidoesters). In other embodiments, the function-

alization element **230** includes carboxylic acid groups that can be coupled via the following bonds and associated electrophilic agents: Ester bonds (Diazoalkanes and Diazoacetyl compounds); Amide bonds (Carbonyldiimidazoles, carbodiimides). In other embodiments, the functionalization element **230** includes hydroxyl groups that can be coupled via the following bonds and associated electrophilic agents: carbamate linkage (carbonyldiimidazole, N,N'-Disuccinimidyl Carbonate (DSC) and N-Hydroxysuccinimidyl chloroformates. Isocyanates) and Ether bonds (Epoxides and Oxiranes). It should be understood that a functionalization element **230** can be attached or bond to the second linking element **220** in various ways.

Referring to FIG. 3 and with further reference to FIGS. 4A-F, one embodiment of a method **300** for functionalizing or preparing a resonant micro-cavity **200** for use as a sensor utilizing click chemistry **250** involves a [3+2]cycloaddition reaction **450** of an azide functional group **410** of the first linking element **210** that binds to an outer surface **202** of the micro-cavity **200** and an alkyne functional group **420** of the second linking element **220** to which the functionalization element **230** is bound. According to one embodiment, the cycloaddition reaction **450** is a [3+2]cycloaddition reaction. Embodiments may also involve other types of click chemistry **250** reactions including, but not limited to the Diels-Alder [4+2] cycloaddition reaction between a diene and a dienophile. In this embodiment, a diene bonds to the outer surface **202** while a dienophile is attached to a functionalization element **230** or probing molecule. In the illustrated embodiment, the functionalization method **300** involves treating the outer surface **202** of the resonant micro-cavity **200** in preparation for binding **205** of the first linking element **210** to the outer surface **202** at step **305**.

As discussed with reference to FIG. 1, step **305** may involve treating or activating an outer silica surface **202** using a Piranha etch solution. At step **310**, the resonant micro-cavity is placed in a solution or aqueous environment. At step **315**, the first linking element **210** having the azide functional group **410** is synthesized or prepared (if necessary) and introduced into the solution or aqueous environment in which the resonant micro-cavity **200** is placed. As a result, in step **320**, a covalent bond **205** is formed between the first linking element **210** having the azide functional group **410** and the active outer surface **202** of the resonant micro-cavity **200**. At step **325**, the second linking element **220** having the alkyne functional group **420** is synthesized or prepared (if necessary) and introduced into the solution or aqueous environment. At step **330**, a covalent bond **452** is formed between the alkyne functional group **420** and the azide functional group **410** as a result of a [3+2]cycloaddition reaction **450**. At step **335**, a functionalization element **230** for sensing a target molecule **240** is introduced into the solution or aqueous environment, and at step **340**, the functionalization element **230** bonds or is attached **225** to the second linking element **220**. FIGS. 4C-F illustrate that embodiments involving a [3+2]cycloaddition reaction **450** may involve a functionalization element **230** that is an antibody (FIG. 4C), an antibody fragment (Fab, Fc) (FIG. 4D); an antigen (FIG. 4E), or a protein (FIG. 4F), and various target molecules **240** may be detected as discussed above.

The manner in which a target molecule **240** attaches or binds **242** to the outer surface **202** via first and second linking elements **210**, **220** as described with reference to FIGS. 1-4F provides for improved flexibility to target several different target molecules **240** in an environmentally benign and stable manner. Further, since embodiments utilize covalent bonding, they are very stable, e.g., stable in the presence of tem-

perature and pH changes. Embodiments provide the ability to control environmental conditions to controllably release target molecules **240** from the functionalized outer surface **202**. In this manner, surface functionalization embodiments allow a resonant micro-cavity sensor **200** having a functionalized outer surface **202** to be reused for subsequent detection or sensing.

The first and second linking elements **210**, **220** can be synthesized using various materials. According to one embodiment, the first linking element **210** and the second linking element **220** are synthesized using the same polymer, and the ends of the polymer are functionalized to synthesize both linking elements **210**, **220**. According to one embodiment, the polymer used for this purpose has a molecular weight greater than 100, examples of which include polyethylene glycol (PEG), polyethylene oxide (PEO) and other suitable polymers having sufficiently long chain lengths and ends that can be functionalized. For ease of explanation, reference is made to a PEG polymer or a polymer generally, but it should be understood that other polymers having sufficiently long chain lengths can be utilized to synthesize first and second linking elements **210**, **220**.

In other embodiments, the first and second linking elements **210**, **220** are made of different types of polymers. According to one embodiment, the first and second linking elements **210**, **220** for use in embodiments described with reference to FIGS. 1-4F are synthesized from a PEG polymer having functionalized ends such that a molecular weight (MW) of a polymer chain of the first linking element **210** is greater than about 300, and a molecular weight of a polymer chain of the second linking element **220** is greater than 1500. Other embodiments may involve other molecular weights that are greater than 100, and molecular weights of 300 and 1500 are provided as examples of how embodiments may be implemented.

In this particular embodiment, the 300 MW first linking element **210** having the azide functional group **410** is covalently bonded **205** to the treated outer surface **202** of the micro-cavity **200**, and the alkyne functional group **420** of the 1500 MW second linking element **220** having an attached functionalization element **230** is covalently bonded **452** to the azide functional group **410** via a cycloaddition reaction **450**. Embodiments that utilize these types of reactions and covalent bonds provide controlled, irreversible bonding such that only the azide group **410** and the alkyne group **420** bind to each other by click chemistry **250**, e.g., a cycloaddition reaction **450**. Thus, the synthesized, non-biological azide group **410** will not bind to other components of a biological solution. Thus, even if alkyne functional groups **420** do not saturate or bind with all of the available azide groups **410**, empty or passive azide **410** binding sites remain empty or unbound due to their selective binding. As a result, other biological elements will not bind to these azide sites **410** given the differences in the chemical structures of the azide functional group **410** and biological elements, thereby reducing or eliminating incorrect or inadvertent binding, which may otherwise reduce the effectiveness of the sensor.

Surface functionalization embodiments can be applied to micro-cavities **200** of various shapes, sizes and configurations may be utilized in embodiments and may be made of various materials. In certain embodiments, the outer surface **202** of a semiconductor micro-cavity **200** is functionalized as described above. In a further embodiment, a micro-cavity **200** that is made of an insulator material is functionalized. In certain embodiments, the micro-cavity **200** is made of silicon, silica (as described above with reference to the Piranha silica surface treatment), glass or silicon nitride.

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Micro-cavities **200** that may be functionalized using click chemistry **250** or a cycloaddition reaction **450** can have a planar shape, e.g., in the form of a disk, a ring or a toroid. For example, FIG. **5** is a scanning electron micro-graph of a planar, toroid-shaped micro-cavity **500**, one example of which is described in U.S. application Ser. No. 10/678,354, the contents of which were previously incorporated herein by reference. One suitable toroid-shaped micro-cavity **500** that may be functionalized according to embodiments is made of silica and is supported by a silicon substrate **510**. The radius of a toroid-shaped micro-cavity **500** may, for example, be about 15 to 100 micrometers, e.g., about 45 micrometers, and may have high Q values and ultra-high Q values (greater than 10^6). In the illustrated example, the substrate **510** is tapered such that the micro-cavity **500** in which optical energy **260** resonates extends outwardly beyond the outer edge or top of the substrate **510**.

Referring to FIG. **6** and with further reference to FIGS. **7A-C**, one method **600** of fabricating a toroid-shaped micro-cavity **500** supported by a substrate **510** as shown in FIG. **5** includes step **602** of wet etching a photolithography patterned silica or silicon dioxide (SiO_2) disk or circular pad **702** on a silicon substrate **704** or other suitable substrate (FIG. **7A**). This may be done using a hydrogen fluoride (HF) solution or other suitable etchant. In step **604**, the silica disk **702** is exposed to a second etchant such as xenon difluoride (XeF_2) gas. XeF_2 is an etchant with high selectivity that is currently utilized to produce, for example, Micro-Electrical Mechanical Systems (MEMS) devices. XeF_2 gas removes or etches portions of the silicon base **704** beneath the periphery of the silica disk **702** (FIG. **6B**), thereby forming the tapered silicon support **510**. In step **606**, a laser, such as an Eximer or CO_2 laser, is applied to the undercut periphery of the silica disk **702** (FIG. **7C**). As a result, the periphery portions of the silica disk **702** are melted or partially or completely liquefied to reflow and form a toroid-shaped micro-cavity **500** having ultra smooth surfaces (FIGS. **5** and **7C**). Further aspects of toroid-shaped micro-cavities **500** and methods of fabrication are described in U.S. application Ser. Nos. 10/678,354 and 11/733,480, the contents of which were previously incorporated herein by reference.

After the micro-cavity **200**, such as the toroid-shaped micro-cavity **500** described above, is fabricated, and the outer surface **202** is functionalized by click chemistry **250** or a cycloaddition reaction **450**, the outer surface **202** of the micro-cavity **200** is sensitized and ready for detection of target molecules **240** of interest based on changes of optical energy **260** resonating within the micro-cavity **200**. Detection of molecules **240** and even detection of a single molecule **240** is accomplished by highly sensitive micro-cavities **200**, e.g., having high or ultra-high Q values, that have a very specific outer surface **202** that is functionalized according to embodiments utilizing click chemistry **250** or a cycloaddition reaction **450**.

Referring again to FIGS. **2A** and **4A**, and with further reference to FIG. **8**, a resonant micro-cavity **200** having a surface **202** functionalized according to embodiments may be part of a sensor system **800**. In the illustrated embodiment, the system **800** includes a light source **810**, such as a laser, which provides optical energy **260** that is coupled into the micro-cavity **200** via a coupler **820**. An optical property of optical energy **260** that evanesces beyond the micro-cavity **200** may be monitored or detected to determine whether a target molecule **240** has bound to the functionalized outer surface **202**. More particularly, a resonant micro-cavity **200** having an outer surface **202** functionalized according to embodiments is operable as a sensor based on a change of an optical property

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of the optical energy **260** resonating within the micro-cavity **200** caused by a target molecule **240** binding **242** to the functionalized outer surface **202**.

In the illustrated embodiment, the micro-cavity **200** is a toroid-shaped micro-cavity **500**. The wavelength of optical energy **260** may change as a result of one or more molecules **240**, and even a single molecule **240**, binding **242** to a functionalized outer surface **202** of the micro-cavity **200**. Further, when a single molecule **240** or multiple molecules **240** interact with the evanescent field of the optical energy **260**, the micro-cavity **200** may be heated, thereby changing the refractive index of the resonating optical energy **260**. In this manner, sensors **200** having an outer surface **202** functionalized according to embodiments can detect small numbers of molecules **240**, and even a single molecule **240**, without the need to label the target molecule(s) **240** beforehand, as is required in various known single molecule sensors. Changes of other optical properties may also be utilized including, for example, changes of polarization.

Referring to FIG. **9**, one example of a coupler **820** that may be used in the system **800** shown in FIG. **8** is in the form of a transmission media or fiber coupler **910** that is coupled to a light source or laser **810**. Light or optical energy **260** emitted by the laser **810** is coupled into the functionalized micro-cavity **200**, e.g., a functionalized toroid-shaped micro-cavity **500** as illustrated, using the fiber coupler **820**. In one known coupler **820**, the transmission media **910** is a tapered waveguide as shown in FIG. **9**, although other waveguide configurations can also be utilized. Tapered sections **912** and the intermediate waist region **914** of the waveguide **910** may be provided, as is known, by stretching a fiber (e.g., a single mode fiber) under controllable tension as it is softened by one or more fixed or movable heat sources (e.g., torches). The diameter of the tapered waist region **914** may be several micrometers, e.g., about 2 micrometers. The toroid-shaped micro-cavity **500**, which may be an ultra-high Q micro-cavity, is coupled to the waist region **914** of the fiber **910**. The diameter of the waist region **914** can be adjusted to properly phase-match to the toroid-shaped micro-cavity **500**.

A light source or optical pump **810** such as a laser is optically connected to a first end **911** of the fiber **910**. The optical pump **810** transmits a signal or optical energy **260** along the fiber **910** through the fiber taper **912** and the waist region **914** where it is coupled into the toroid-shaped micro-cavity **500**. Evanescent optical energy **260** that emanates from the waist region **914** is coupled into the toroid-shaped micro-cavity **500** such that one or more excited laser signals circulate or resonate within the toroid-shaped micro-cavity **500** with effectively total internal reflection and with minimal internal attenuation and radiative losses, e.g., in a Whispering Gallery Mode (WGM) or other resonant mode. A portion of the resonant optical energy **260** evanesces beyond the micro-cavity **500** and is presented for coupling back into the waveguide waist **914**, through an outgoing tapered region **912** and into the outgoing end **913** of the fiber **910**. Further aspects of a suitable coupler **900** for use in embodiments are described in U.S. Pat. No. 6,741,628 to Painter et al., the contents of which are incorporated herein by reference.

Although various figures illustrate a single resonant micro-cavity sensor **200** having a single micro-cavity, such as a toroid-shaped micro-cavity **500**, other embodiments are directed to an array of resonant micro-cavity sensors **200** that are coupled to one or more or respective couplers **820** or waveguides. An array of sensors **200** may have outer surfaces **202** that are functionalized according to embodiments and the same or different shapes and/or sizes, the same or different resonant wavelengths and may be configured for high

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throughput detection of multiple gases or vapors. Micro-cavities **200** of an array may be made of the same material or different materials and may include the same or different surface functionalization elements **230**. For ease of explanation and illustration, reference is made to an individual resonant micro-cavity sensor **200**, but other embodiments may include arrays of various numbers of sensors **200** that can be structured in different manners.

Additionally, although certain embodiments are described with reference to a toroid-shaped micro-cavity **500**, sensor embodiments and arrays thereof may also be implemented using micro-cavities **200** of other shapes, sizes, and materials. For example, referring to FIG. **10**, a resonant micro-cavity sensor **200** in the form of a spherical micro-cavity or micro-sphere **1000** may be functionalized using click chemistry **250** or a cycloaddition reaction **450**. One example of a micro-sphere **1000** that may be utilized with surface functionalization embodiments is described in U.S. Pat. No. 6,741,628, the contents of which were previously incorporated herein by reference.

One manner of fabricating a micro-sphere **1000** for use in embodiments involves melting a small piece of glass material, e.g., phosphate glass, in a crucible. While the phosphate is molten, the tip of a silica fiber taper, which has a higher melting point, is placed into the melt. As the silica "stem" is extracted, a small phosphate taper is formed on the end of the silica taper. A laser is used to melt the end of the phosphate taper, forming a sphere under surface tension. The silica fiber stem is finally placed in a fiber chuck and used as a handling rod to control and position the phosphate sphere. The micro-sphere **1000** may be made of silica and other suitable materials, and may have a diameter of about 100 micrometers to about 3 millimeters, e.g., about 1 millimeter. Other micro-sphere **1000** materials and dimensions and thicknesses may be utilized, e.g., as discussed above with respect to the toroid-shaped micro-cavity **500**. The outer surface **1002** of the micro-sphere **1000** may then be functionalized in a similar manner as described above with reference to FIGS. **1-4F** and be integrated into sensor system or within an array of sensors as described above.

Further, the Q value and sensitivity of resonant micro-cavity sensor **200** having a functionalized outer surface **202** according to embodiments can vary and can be configured to detect trace amounts of different target molecules **240** in an aqueous or air environment. For example in certain embodiments, a gas or vapor sensor **200** constructed according to one embodiment having a toroid-shaped micro-cavity **500** has an ultra-high Q value of greater than 10^6 , e.g., 10^7 and greater than 10^8 . Spherical micro-cavities **1000** may have similar Q values.

FIGS. **11-25B** illustrate certain embodiments of first and second linking elements **210**, **220**, fluorescent counterparts to the linking elements **210**, **220** that are synthesized for purposes of testing, and summaries of different fluorescence tests that were performed.

FIG. **11** illustrates one embodiment of a method for synthesizing a first linking element **210** having an azide functional group **410**. In the illustrated embodiment, an initial or starting compound or material **1100** including triethoxysilane ((EtO)₃Si) **1102**, a polymer such as PEG **1104** and hydrogen **1106** is placed in a solution **1110**. According to one embodiment, the solution is a mixture of sodium azide (NaN₃) **1112** and dimethylformamide (DMF) **1114** and at a temperature of about 50° C. The resulting reaction of the initial compound **1100** and the solution **1110** leads to synthesis of a first linking element **210**. In the illustrated embodiment, the first linking

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element **210** comprises triethoxysilane ((EtO)₃Si) **1102**, the polymer (PEG) **1104**, and the azide functional group N₃ **410**.

FIG. **12** illustrates how a fluorescently labeled counterpart **1220** to the first linking element **210** as shown in FIG. **11** can be synthesized for purposes of testing and verifying embodiments. As explained above, embodiments function without the need for labeled molecules, but the fluorescently labeled counterpart **1220** is synthesized for conducting verification tests involving fluorescence intensity as described in further detail below.

In the illustrated example, and with further reference to FIG. **13**, an initial or starting compound **1200** including triethoxysilane ((EtO)₃Si) **1102**, a polymer such as PEG **1104** and NH₂ **1206** is placed in a solution **1210** that is a mixture of tetramethyl rhodamine Iso-Thiocyanate (TRITC) **1212** (illustrated in further detail in FIG. **13**) and DMF **1114** at room temperature (RT). The resulting reaction of the compound **1200** and the solution **1210** leads to synthesis of a fluorescently labeled counterpart **1220** to the first linking element **210**. As shown in FIG. **12**, the fluorescently labeled counterpart **12220** includes ((EtO)₃Si) **1102**, the polymer **1104**, TRITC **1212** and associated nitrogen, hydrogen and sulfur elements. TRITC **1212** allows the counterpart **1220** to be used in tests involving analysis of fluorescence intensity.

FIGS. **14** and **15** illustrate an embodiment of a method for synthesizing a second linking element **220** having an alkyne functional group **420**. In the illustrated embodiment, an initial compound **1400** (illustrated in further detail in FIG. **15**) including malamite (MAL) **1402**, a polymer **1104** such as PEG₂₄ or another suitable polymer, and a NHS group **1404** is placed in a solution **1410**. In one embodiment, the solution **1410** may be a mixture of propargylamine **1412** and 0.1M sodium bicarbonate (NaHCO₃) **1414** at 25° C. The resulting reaction of the compound **1400** and the solution **1410** leads to synthesis of a second linking element **220** including MAL **1402**, the polymer **1104** and the alkyne functional group **420**. In the embodiments illustrated in FIGS. **11** and **14**, the azide functional group **410** of the first linking element **210** and the alkyne functional group **420** of the second linking element **220** bond together by click chemistry **250**, e.g. by a cycloaddition reaction **450**.

FIGS. **16** and **17** illustrate how a fluorescently labeled counterpart **1650** to the second linking element **220** as shown in FIG. **14** can be synthesized. As explained above, embodiments are operable without the need for labeled molecules, but the fluorescently labeled counterpart **1650** is synthesized and utilized to verify the effectiveness of embodiments utilizing fluorescence intensity testing, as described in further detail below.

In the illustrated example, an initial compound **1600** (as shown in FIG. **17**) including Fluorenylmethoxycarbonyl (Fmoc) **1602**, a polymer **1104** such as PEG₇₇ or another suitable polymer, and a NHS group **1404** is placed in a first solution **1610**. The solution **1610** may be a mixture of propargylamine **1412** and 0.1M sodium bicarbonate (NaHCO₃) **1414** at room temperature (RT). The compound resulting from that reaction is then placed in a second solution **1620**, which is 20% piperidine **1622** in a DMF **1114** solution at room temperature (RT), thereby forming an intermediate compound **1630**, which has an alkyne functional group **1632**. The intermediate compound **1630** is then placed in a solution **1640** that is a mixture of TRITC **1212** (as shown in FIG. **13**) and DMF **1114** at room temperature (RT). The resulting reaction of the intermediate compound **1630** and the solution **1640** leads to synthesis of a fluorescently labeled counterpart **1650** to the second linking element **220**. As shown in FIG. **16**,

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the counterpart **1650** includes a polymer **1104**, TRITC **1212** for fluorescence studies and the alkyne functional group **420**.

Having synthesized the first linking element **210** (FIG. **11**), the second linking element **220** (FIG. **14**), and their respective fluorescent counterparts **1220**, **1650** (FIGS. **12** and **16**), the structure of the linking elements **210**, **220** was analyzed utilizing nuclear magnetic resonance spectroscopy to verify the structure of the linking elements **210**, **220**, and which demonstrated that the structure was dominated by a PEG chain. Details of other tests involving the synthesized linking elements **210**, **220** and a silica toroid-shaped micro-cavity **500** (as described with reference to FIGS. **5-7C**) are described with reference to FIGS. **18-25B**.

Referring to FIGS. **18-19**, to determine acceptable or optimum bonding reaction conditions of the first linking element **210** to the outer silica surface **202** of a toroid-shaped micro-cavity **500**, the outer surfaces **202** of three groups of toroid-shaped micro-cavities **500** were treated using a Piranha etch solution of 70% sulfuric acid (H_2SO_4) (**1802**) and 30% hydrogen peroxide (H_2O_2) (**1804**) for about 15 minutes. Samples of the fluorescent counterpart **1220** (FIG. **12**) to the first linking element **210** were prepared. Following the etch treatment **1800**, the fluorescent counterpart **1220** to the first linking element **210** was bound to the treated outer surface **202** by placing the treated micro-cavities **500** in a solution **1110** that is a mixture of sodium azide (NaN_3) **1112** and DMF **1114** for different lengths of time.

More particularly, a first sample or group of 35 micro-cavities **500** was prepared by binding a fluorescent counterpart **1220** to the first linking element **210** to the outer surface **202** of the toroid-shaped micro-cavities **500** by placing them in solution **1110** having a concentration of about 5 mg/ml and a temperature of about 50° C. for about 5 hours. A second sample or group of 35 micro-cavities **500** was placed in a solution **1110** having a concentration of about 5 mg/ml and a temperature of about 50° C. for about 1 hour. A third sample or group of 35 micro-cavities **500** was placed in a solution **1110** having a concentration of about 5 mg/ml and a temperature of about 50° C. for about 40 minutes.

FIGS. **20A-C** and **21A-C** graphically illustrate data resulting from measuring the fluorescence intensity along different positions (microns) on the circumference of the outer surface **202** of each micro-cavity **500** in each of the three groups prepared as described above. The fluorescence data for the first group (5 hours in solution **1110**) are plotted in FIGS. **20A** and **21A**, the fluorescence data for the second group (1 hour in solution **1110**) are plotted in FIGS. **20B** and **21B**, and the fluorescence data for the third group (40 minutes in solution **1110**) are plotted in FIGS. **20C** and **21C**. As shown in these figures, the toroid-shaped micro-cavities **500** fabricated using a solution time of 40 minutes (FIGS. **20C** and **21C**) exhibited the least amount of noise or variance, thus demonstrating that these method parameters resulted in the most uniform binding of the fluorescent counterpart **1220** of the first linking element **210** to the outer surface **202** of the micro-cavity **500**. Based on these results, it can be inferred that a similar method can be used for uniform binding of the first linking element **210** to the outer surface **202** of a micro-cavity **200**, including a toroid-shaped micro-cavity **500**. More particularly, referring to FIGS. **20A-C**, clumps, i.e., oligomeric TRITC-silanes or locally π -stacked TRITC **1212**, can be reduced using shorter reaction times (e.g., about 40 minutes in solution rather than 1 or 5 hours), and FIGS. **21A-C** illustrate that the geometric means around the toroid-shaped micro-cavity **500** show a minimal intensity variation over the entire toroid

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surface **202** from sample to sample, and that longer reaction times and higher concentrations may not provide significant advantages.

Referring to FIG. **22**, additional experiments were performed to check for auto-fluorescence of toroid-shaped micro-cavity **500** samples prepared to having both of the first and second linking elements **210**, **220** rather than only the first linking element **210** and possible binding without catalysts. As shown in FIG. **22**, an outer surface **202** of a toroid-shaped micro-cavity **500** was treated using a Piranha etch solution as described above to activate the outer surface **202**. The micro-cavity **500** was placed in a solution **2210** having 0.5 mg/ml concentration of EtOH **2212** at 40° C. for about 40 minutes, thereby resulting in bonding of a first linking element **210** having an azide functional group (N_3) **410** to the outer surface **202** of the micro-cavity **500**. The micro-cavity **500** having the azide functional group **410** was then placed in a solution **2220** containing copper sulfate (CuSO_4) **2222**, tris(2-carboxy-ethyl)phosphine) (TCEP) **2223**, a solvent tert-butyl alcohol (t-BuOH) **2224**, 50 mM lead sulfide **2225** and tris(azoly)amine 2 mM in a dimethyl sulfoxide (DMSO) **2226** solvent at room temperature (RT) for about five hours. The click reaction **250** may also be controlled without copper sulfate (CuSO_4), TCEP and tris(azoly)amine. For example, the solution utilized may include t-BuOH, PBS 50 mM at room temperature for 5 hours.

The reaction of the treated outer surface **202** and the solution **2220** results in a click chemistry **250** or cycloaddition reaction **450** such that the a molecular structure including the first linking element **210** having the azide functional group (N_3) **410**, a second linking element **220** having an alkyne functional group **420** and a TRITC molecule **1212**. During this test, TRITC **1212** was introduced after applying the first linking element **210** and after applying the second linking element **220**. As a result, at each of these points, TRITC **1212** was introduced such that the end groups of the linking elements **210**, **220** were replaced with TRITC **1212**, thereby resulting in the molecular structure shown in FIG. **22** in which TRITC **1212** replaces an end group of the alkyne functional group **420** for use in fluorescence testing to demonstrate the effectiveness of embodiments.

FIGS. **23A-C** are graphs of data illustrating fluorescence intensity relative to a circumferential position along an outer surface **202** of the toroid-shaped micro-cavity **500** that is functionalized using both first and second linking elements **210**, **220** and click chemistry **250**. FIG. **23A** illustrates raw fluorescence intensity data relative to a circumferential position along the outer surface **202**. FIG. **23B** illustrates the data shown in FIG. **23A** but with clumps, micelles, or spheres of molecules removed from the outer surface **202**, thereby demonstrating uniformity based on the presence of minimal micelles on the outer surface **202**. FIG. **23C** illustrates the geometric mean of the fluorescence intensity relative to the circumferential position along the outer surface **202**. The geometric mean data shown in FIG. **23C** illustrates minimal intensity variation over the entire outer circumferential surface **202**.

Referring to FIGS. **24-25B**, another test involved analyzing the quality (Q) factor of optical energy **260** resonating within a toroid-shaped micro-cavity **500** functionalized with both first and second linking elements **210**, **220** and malamite (MAL) **2430**, to which functionalization elements **230** can be attached. Tests were performed using micro-cavity **500** functionalized as shown in FIG. **24** to verify that the first and second linking elements **210**, **220** do not negatively impact Q factor or do so to a negligible or acceptable degree.

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Referring to FIG. 24, outer surfaces 202 of multiple toroid-shaped micro-cavities 500 were treated using a Piranha etch solution and then placed in a solution 2410 having 0.5 mg/ml concentration of EtOH 2212 at 40° C. for about 40 minutes, thereby resulting in bonding of the first linking element 210 having an azide functional group (N_3) 410 to the outer surfaces 202 of the micro-cavities 500. The micro-cavities 500 having the first linking element 210 were then placed in a solution 2420 containing copper sulfate ($CuSO_4$) 2222, tris (2-carboxyethyl)phosphine (TCEP) 2223, a solvent tert-butyl alcohol (t-BuOH) 2224, 50 mM lead sulfide 2225 and tris triazolylamine 2 mM in a dimethyl sulfoxide (DMSO) 2226 solvent at room temperature (RT) for about five hours, as described above with reference to FIG. 22. The reaction of the solution 2420 and the treated outer surfaces 202 having the first linking element 210 resulted in a click chemistry 250 or cycloaddition reaction 450 of the azide functional group (N_3) 410 of the first linking element 210 and the alkyne functional group 420 of the second linking element 220, which is mixed in the reaction with the solution 2220 to form a TRITC 1212 labeled counterpart 1650 linked to the first linking element 210 via cyclic ring. Alternatively, the reaction may be carried out without copper sulfate ($CuSO_4$), TCEP and tris triazolylamine. For example, the solution 2420 utilized may include t-BuOH, PBS 50 mM at room temperature for 5 hours. Malamite (MAL) 2430 is attached to the second linking element 220, in a manner that is similar to how a functionalization element 230 for sensing a target molecule 240 would be attached to the second linking element 220.

FIGS. 25A-B are graphs plotting Q factor data for the micro-cavities functionalized as shown in FIG. 24. FIG. 25A illustrates Q factor data for a toroid-shaped micro-cavity 500 after binding of the first linking element 210 to the outer surface 202. FIG. 25B illustrates Q factor data for a toroid-shaped micro-cavity 500 after binding of the second linking element 220 to the first linking element 210.

As shown in FIGS. 25A-B, the Q factor is not impacted, or is impacted by a small amount, thereby demonstrating that surface functionalization embodiments do not impact Q factor or do so to a minimal or negligible degree. More particularly, it was determined that the average reduction of Q factor upon addition of the first linking element 210 to the outer surface 202 was about 15%, and the combined average Q factor reduction upon binding of the second linking element 220 was about 20%. The smallest Q factor reduction that was observed was about 2%. Thus, these experiments demonstrated the effectiveness of embodiments and that embodiments are useful for functionalizing outer surfaces of high Q and ultra-high Q micro-cavities.

Although references have been made in the foregoing description to various embodiments, persons of ordinary skill in the art will recognize that insubstantial modifications, alterations, and substitutions can be made to the described embodiments without departing from the invention as recited in the accompanying claims.

For example, embodiments may involve resonant micro-cavities that are made of various resonator materials and may have various shapes and sizes. Further, arrays of sensors may have various numbers of sensors, which may have the same or different micro-cavities and deformable coatings. Embodiments may involve various types of functionalization elements to detect certain target molecules.

Additionally, various surface treatments may be used to activate the outer surface for binding of the first linking element. The linking elements may also be formed or made from various polymers, which may be the same or different polymers. Polymers of various molecular weights may be utilized.

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Synthesis parameters may also be adjusted as necessary. Further, various types of click chemistry and cycloaddition reactions may be utilized. Additionally, various types of bonds or linkages may be formed between a second linking element and a functionalization element, which may be used to detect various types of target molecules, including single molecules.

Moreover, in other embodiments, an outer surface of a micro-cavity can be partially functionalized (e.g., 75% functionalized), and after a target molecule is identified, the remaining surface can be functionalized for a later identified target molecule.

Additionally, where methods and steps described above indicate certain events occurring in certain order, it should be understood upon reading this disclosure that the ordering of certain steps may be modified and that such modifications are in accordance with the variations of the invention. Certain steps may be performed concurrently in a parallel or performed sequentially as described above. For example, although embodiments are described with reference to a sequence of a first linking element bonding to a resonator surface, a second linking element bonding to the first linking element, and a functionalization element bonding to the second linking element, other embodiments involve binding of the functionalization element to the second linking element, and then binding of the second linking element to the first linking element, before or after the first linking element binds to the outer surface of the micro-resonator. Accordingly, it should be understood that the sequence of steps illustrated in various figures are provided for purposes of explanation and illustration and in a non-limiting manner, and that various steps and reactions may occur in different orders.

Thus, it should be understood that the invention generally, as well as the specific embodiments described herein, are not limited to the particular forms or methods disclosed, but also cover all modifications, equivalents and alternatives falling within the scope of the appended claims.

What is claimed is:

1. A resonant micro-cavity sensor, comprising:

a resonant micro-cavity having an outer surface and a Q factor greater than 10^8 ;
a first polymer linking element bound to the outer surface;
a second polymer linking element bound to the first linking element by click chemistry and
a functionalization element for sensing a target molecule, the functionalization element being bound to the second linking element.

2. The sensor of claim 1, wherein the functionalization element is an antibody, an antibody fragment, an antigen or a protein.

3. The sensor of claim 1, wherein the first polymer linking element and the second polymer linking element form a substantially uniform single layer.

4. The sensor of claim 1, wherein respective polymer chains of the first polymer linking element and the second polymer linking element have respective molecular weights greater than 100.

5. The sensor of claim 1, wherein a molecular weight of a polymer chain of the first polymer linking element is greater than about 300, and a molecular weight of a polymer chain of the second polymer linking element is greater than 1500.

6. The sensor of claim 1, wherein the resonant micro-cavity is a planar micro-cavity.

7. A resonant micro-cavity sensor, comprising:

a resonant micro-cavity having an outer surface and a Q factor greater than 10^8 ;
a first polymer linking element bound to the outer surface and having a first functional group;

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a second polymer linking element having a second functional group, wherein a bond is formed between the first functional group and the second functional group as a result of a cycloaddition reaction, and

a functionalization element for detecting a target molecule, wherein the functionalization element is bound to the second linking element.

8. The sensor of claim 7, wherein the functionalization element is an antibody, an antibody fragment, an antigen or a protein.

9. The sensor of claim 7, wherein the first polymer linking element and the second polymer linking element form a substantially uniform single layer.

10. The sensor of claim 7, at least one of the first linking polymer element and the second polymer linking element is made of a polyethylene glycol polymer.

11. The sensor of claim 7, wherein the first polymer linking element and the second polymer linking element have respective polymer chains of respective molecular weights greater than 100.

12. The sensor of claim 10, wherein a molecular weight of a polymer chain of the first polymer linking element is greater than about 300, and a molecular weight of a polymer chain of the second polymer linking element is greater than 1500.

13. The sensor of claim 7, wherein a covalent bond is formed between the first functional group and the second functional group.

14. The sensor of claim 7, wherein the first polymer linking element and the second polymer linking elements are bonded to each other by a cycloaddition reaction of an azide group of the first polymer linking element and an alkyne group of the second polymer linking element.

15. A resonant micro-cavity sensor, comprising:

a resonant micro-cavity having an outer surface and a Q factor greater 10^8 ;

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a first polymer linking element bound to the outer surface and having an azide functional group, a polymer chain of the first polymer linking element having a molecular weight greater than 100;

a second polymer linking element having alkyne functional group, wherein a bond is formed between the azide functional group and the alkyne functional group as a result of a cycloaddition reaction, a polymer chain of the second polymer linking element having a molecular weight greater than 100; and

a functionalization element for detecting a target molecule, wherein the functionalization element is bound to the second polymer linking element.

16. The sensor of claim 15, wherein the functionalization element is an antibody, an antibody fragment, an antigen or a protein.

17. The sensor of claim 15, wherein the molecular weight of a polymer chain of the first polymer linking element is greater than about 300, and the molecular weight of a polymer chain of the second polymer linking element is greater than 1500.

18. The sensor of claim 1, at least one of the first linking polymer element and the second polymer linking element comprising a polyethylene glycol polymer, wherein a molecular weight of a polymer chain of the first linking element is at least 300, and a molecular weight of a polymer chain of the second polymer linking element is at least 1500.

19. The sensor of claim 15, at least one of the first linking polymer element and the second polymer linking element comprising a polyethylene glycol polymer.

20. The sensor of claim 1, at least one of the first linking polymer element and the second polymer linking element comprising a polyethylene oxide polymer.

21. The sensor of claim 15, at least one of the first linking polymer element and the second polymer linking element comprising a polyethylene oxide polymer.

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